



HAL
open science

International Benchmark for Total Metabolic Tumor Volume Measurement in Baseline 18 F-FDG PET/CT of Lymphoma Patients: A Milestone Toward Clinical Implementation

Ronald Boellaard, Irène Buvat, Christophe Nioche, Luca Ceriani, Anne-Ségolène Cottereau, Luca Guerra, Rodney J Hicks, Salim Kanoun, Carsten Kobe, Annika Loft, et al.

► To cite this version:

Ronald Boellaard, Irène Buvat, Christophe Nioche, Luca Ceriani, Anne-Ségolène Cottereau, et al.. International Benchmark for Total Metabolic Tumor Volume Measurement in Baseline 18 F-FDG PET/CT of Lymphoma Patients: A Milestone Toward Clinical Implementation. *Journal of Nuclear Medicine*, 2024, 65 (9), pp.1343-1348. 10.2967/jnumed.124.267789 . inserm-04783144

HAL Id: inserm-04783144

<https://inserm.hal.science/inserm-04783144v1>

Submitted on 14 Nov 2024

HAL is a multi-disciplinary open access archive for the deposit and dissemination of scientific research documents, whether they are published or not. The documents may come from teaching and research institutions in France or abroad, or from public or private research centers.

L'archive ouverte pluridisciplinaire **HAL**, est destinée au dépôt et à la diffusion de documents scientifiques de niveau recherche, publiés ou non, émanant des établissements d'enseignement et de recherche français ou étrangers, des laboratoires publics ou privés.



Distributed under a Creative Commons Attribution 4.0 International License

International Benchmark for Total Metabolic Tumor Volume Measurement in Baseline ¹⁸F-FDG PET/CT of Lymphoma Patients: A Milestone Toward Clinical Implementation

Ronald Boellaard*¹, Irène Buvat*², Christophe Nioche², Luca Ceriani³, Anne-Ségolène Cottureau⁴, Luca Guerra^{5,6}, Rodney J. Hicks⁷, Salim Kanoun⁸, Carsten Kobe⁹, Annika Loft¹⁰, Heiko Schöder¹¹, Annibale Versari¹², Conrad-Amadeus Voltin⁹, Gerben J.C. Zwezerijnen¹, José M. Zijlstra¹³, N. George Mikhael¹⁴, Andrea Gallamini¹⁵, Tarek C. El-Galaly^{16,17}, Christine Hanoun¹⁸, Stephane Chauvie¹⁹, Romain Ricci²⁰, Emanuele Zucca²¹, Michel Meignan⁴, and Sally F. Barrington²²

¹Department of Radiology and Nuclear Medicine, Amsterdam UMC, Cancer Center Amsterdam, Amsterdam, The Netherlands; ²LITO, Inserm, Institut Curie, Orsay, France; ³Clinic of Nuclear Medicine and PET-CT Centre, Imaging Institute of Southern Switzerland; and EOC, Institute of Oncology Research, Faculty of Biomedical Sciences, Università della Svizzera Italiana, Bellinzona, Switzerland; ⁴Department of Nuclear Medicine, Cochin Hospital, APHP; and Faculté de Médecine, Université Paris Cité, Paris, France; ⁵Nuclear Medicine Unit, Fondazione IRCCS San Gerardo dei Tintori, Monza, Italy; ⁶School of Medicine and Surgery, University of Milano Bicocca, Milan, Italy; ⁷Department of Medicine, St. Vincent's Hospital Medical School, University of Melbourne, Melbourne, Victoria, Australia; ⁸Centre de Recherche Clinique de Toulouse, Team 9, Toulouse, France; ⁹Department of Nuclear Medicine, Faculty of Medicine and University Hospital Cologne, University of Cologne, Cologne, Germany; ¹⁰PET & Cyclotron Unit 3982, Copenhagen University Hospital, Copenhagen, Denmark; ¹¹Molecular Imaging and Therapy Service, Memorial Sloan Kettering Cancer Center, New York, New York; ¹²Nuclear Medicine Department, Azienda Unità Sanitaria Locale-IRCCS, Reggio Emilia, Italy; ¹³Department of Hematology, Amsterdam UMC, Cancer Center Amsterdam, Amsterdam, The Netherlands; ¹⁴Department of Clinical Oncology, Guy's Cancer Centre and School of Cancer and Pharmaceutical Sciences, King's College London University, London, United Kingdom; ¹⁵Research and Innovation Department, Antoine Lacassagne Cancer Center, Nice, France; ¹⁶Department of Hematology, Aalborg University Hospital, Aalborg, Denmark; ¹⁷Department of Hematology, Odense University Hospital, Odense, Denmark; ¹⁸Department of Hematology and Stem Cell Transplantation, West German Cancer Center, University Hospital Essen, University of Duisburg-Essen, Essen, Germany; ¹⁹Medical Physics Division, Santa Croce e Carle Hospital, Cuneo, Italy; ²⁰LYSARC, Centre Hospitalier Lyon-Sud, Pierre-Bénite, France; ²¹Oncology Institute of Southern Switzerland; and EOC, Institute of Oncology Research, Faculty of Biomedical Sciences, Università della Svizzera Italiana, Bellinzona, Switzerland; and ²²King's College London and Guy's and St. Thomas's PET Centre, School of Biomedical Engineering and Imaging Sciences, King's College London, London, United Kingdom

Total metabolic tumor volume (TMTV) is prognostic in lymphoma. However, cutoff values for risk stratification vary markedly, according to the tumor delineation method used. We aimed to create a standardized TMTV benchmark dataset allowing TMTV to be tested and applied as a reproducible biomarker. **Methods:** Sixty baseline ¹⁸F-FDG PET/CT scans were identified with a range of disease distributions (20 follicular, 20 Hodgkin, and 20 diffuse large B-cell lymphoma). TMTV was measured by 12 nuclear medicine experts, each analyzing 20 cases split across subtypes, with each case processed by 3–4 readers. LIFEx or ACCURATE software was chosen according to reader preference. Analysis was performed stepwise: TMTV1 with automated preselection of lesions using an SUV of at least 4 and a volume of at least 3 cm³ with single-click removal of physiologic uptake; TMTV2 with additional removal of reactive bone marrow and spleen with single clicks; TMTV3 with manual editing to remove other physiologic uptake, if required; and TMTV4 with optional addition of lesions using mouse clicks with an

SUV of at least 4 (no volume threshold). **Results:** The final TMTV (TMTV4) ranged from 8 to 2,288 cm³, showing excellent agreement among all readers in 87% of cases (52/60) with a difference of less than 10% or less than 10 cm³. In 70% of the cases, TMTV4 equaled TMTV1, requiring no additional reader interaction. Differences in the TMTV4 were exclusively related to reader interpretation of lesion inclusion or physiologic high-uptake region removal, not to the choice of software. For 5 cases, large TMTV differences (>25%) were due to disagreement about inclusion of diffuse splenic uptake. **Conclusion:** The proposed segmentation method enabled highly reproducible TMTV measurements, with minimal reader interaction in 70% of the patients. The inclusion or exclusion of diffuse splenic uptake requires definition of specific criteria according to lymphoma subtype. The publicly available proposed benchmark allows comparison of study results and could serve as a reference to test improvements using other segmentation approaches.

Key Words: total metabolic tumor volume; ¹⁸F-FDG PET/CT; lymphoma; benchmark

J Nucl Med 2024; 65:1343–1348
DOI: 10.2967/jnumed.124.267789

Received Mar. 15, 2024; revision accepted Jun. 21, 2024.
For correspondence or reprints, contact Ronald Boellaard (r.boellaard@amsterdamumc.nl).

*Contributed equally to this work.

Published online Aug. 1, 2024.

Immediate Open Access: Creative Commons Attribution 4.0 International License (CC BY) allows users to share and adapt with attribution, excluding materials credited to previous publications. License: <https://creativecommons.org/licenses/by/4.0/>. Details: <https://jnm.snmjournals.org/page/permissions>.

COPYRIGHT © 2024 by the Society of Nuclear Medicine and Molecular Imaging.

Accurate staging and response assessment are critical for optimal management of lymphoma patients. ¹⁸F-FDG PET/CT is the

current standard for staging and response assessment in ^{18}F -FDG-avid lymphomas (1–5).

Pretreatment total metabolic tumor volume (TMTV), measured using ^{18}F -FDG PET/CT, provides prognostic information, and TMTV, alone or in combination with other clinical risk factors, outperforms commonly used international prognostic scores (2,6–11). TMTV also offers a more accurate reflection of risk than do traditional staging and CT estimates of bulk (10,12). Prognostic models incorporating TMTV can identify high-risk patients who may require more intensive treatment, and treatment-induced changes in TMTV have been proposed to monitor treatment efficacy (13,14).

However, there are technical challenges to adoption of TMTV (15–18). TMTV assessment requires delineation of metabolically active lymphoma lesions in ^{18}F -FDG PET/CT images. The most common segmentation methods use SUV thresholds (e.g., $\text{SUV} \geq 2.5$ or $\text{SUV} \geq 4.0$) or a percentage of the SUV_{max} (e.g., 41% SUV_{max}) (18). Other methods apply majority-vote approaches, gradient analysis, or artificial intelligence (18,19). Several studies (16,17,20) reported that the prognostic performance of TMTV is similar, irrespective of the methods used, suggesting that the choice of the segmentation approach is not critical. The success of generating visually correct TMTV delineations with common segmentation methods has been explored as well as their discriminative power and manual-editing requirements. The SUV4.0 method was considered the most successful for TMTV delineation in patients with diffuse large B-cell lymphoma and Hodgkin lymphoma (21,22).

Although the prognostic performance of TMTV with different segmentation methods seems comparable, TMTV values vary widely depending on the method. Consequently, a generally applicable TMTV cutoff that discriminates high-risk patients from low-risk patients cannot be used (23). Standardization of TMTV measurements is therefore needed, as stressed in an expert consensus paper from 2019 (18). Successful implementation of TMTV as a quantitative biomarker also depends on availability of a quick, easy, and reproducible measurement method with high accuracy. The method should be robust to variation in PET/CT technology and image reconstruction algorithms to ensure reproducible measurements across imaging sites. The SUV4.0 method appears to be the least affected among several PET image reconstruction protocols (24).

The present study aims to develop and provide an international benchmark dataset to standardize TMTV measurements in lymphoma, thereby allowing TMTV to be used as a reproducible biomarker.

MATERIALS AND METHODS

^{18}F -FDG PET/CT Studies

Sixty baseline ^{18}F -FDG PET/CT scans from clinical trials were selected (20 follicular, 20 Hodgkin, and 20 diffuse large B-cell lymphoma patients). These scans were acquired as part of the H10 (Hodgkin), AHL2011 (Hodgkin), FOLL12 (follicular), RELEVANCE (follicular), and LNH2007-3B (B-cell) trials (3,25–28). The institutional review board approved these studies, and all subjects provided written informed consent. The scans were selected as representative of the broad range of ^{18}F -FDG distributions seen in practice (Supplemental Fig. 1; supplemental materials are available at <http://jnm.snmjournals.org>) by an international panel of PET/CT lymphoma experts. Scans included less frequently occurring, but not uncommon, uptake patterns, such as focal or diffuse high uptake in the liver and spleen.

TMTV Assessments

Each panel member assessed 20 cases, balanced between lymphoma subtypes, with each case analyzed by 3–4 readers. TMTVs were measured using LIFEx (29) or ACCURATE (PETRA) software according to reader preference. These software programs were first cross-calibrated by comparing segmentation results for preselection of lesions, with simple removal of physiologic uptake with single clicks and simple addition of tumor uptake by mouse clicks, and by ensuring that TMTVs were equal. One dataset ($n = 20$) was additionally yet independently analyzed using FIJI software (ImageJ) (30).

TMTVs were measured using 4 steps (31). TMTV1 is the automated preselection of lesions using an SUV of at least 4 and a volume of at least 3 cm^3 with a single-mouse-click removal of physiologic uptake (e.g., brain, bladder). TMTV2 is the additional removal of reactive bone marrow and spleen uptake with single clicks, if required. TMTV3 is the additional manual editing to remove any other physiologic uptake, if required (e.g., in which tumor-related and physiologic uptake was in close proximity, such as the ureter and retroperitoneal nodes included by the software as a single volume). TMTV4, or final TMTV, is the same as TMTV3 except it adds lesions with mouse clicks using an SUV of at least 4 (no volume threshold) as an optional step if the reader considered that this was practical and likely to influence the prognostic assessment.

Reader instructions (Supplemental File 1) indicated which scans to analyze and provided advice about what to include in the TMTV, including focal nodal, splenic, and bone marrow uptake and diffuse uptake in the spleen in the absence of similar reactive changes in the bone marrow (18,32–36). Readers were provided with written manuals or movies illustrating the use of the software tools (Supplemental Files 2–4) and a report form (Supplemental File 5).

Comparison of TMTVs

For each scan, the reference value for a given TMTV was defined as the median TMTV provided by the 3 or 4 readers. TMTVs were compared with these reference TMTVs for each patient using correlations and difference plots. In addition, we calculated intraclass correlation coefficients between readers for the provided TMTVs. Cases of large discrepancies between the final TMTVs and the reference value, suggesting reader discrepancy, were visually reviewed by an adjudicator, accounting for readers' comments.

Data Sharing

The 3D PET/CT images and reference TMTV values corresponding to each step (TMTV1, TMTV2, TMTV3, and TMTV4) of the benchmark are provided and can be downloaded from <https://zenodo.org/records/11409717>. Coronal and sagittal maximum-intensity projections with overlaid tumor segmentations are provided as a visual indication of lesions included in the final TMTV.

RESULTS

Figure 1 provides an example of TMTVs obtained at each step. The final TMTV ranged from 8 to $2,288 \text{ cm}^3$ across scans and readers. In 80% of cases, the final TMTV was identical between readers, and in 87% of cases, it was within 10 cm^3 or within 10%. TMTV differences were exclusively related to reader interpretation of lesion inclusion or high-uptake region removal for the final TMTV (Table 1). Two readers repeated the analysis with the ACCURATE and LIFEx software tools and reported identical values. Moreover, an additional analysis with FIJI software (30) using the Beth Israel plug-in provided TMTV values within 10% or within 10 cm^3 of TMTV4 except for the cases listed in Table 1 (Supplemental Fig. 2).

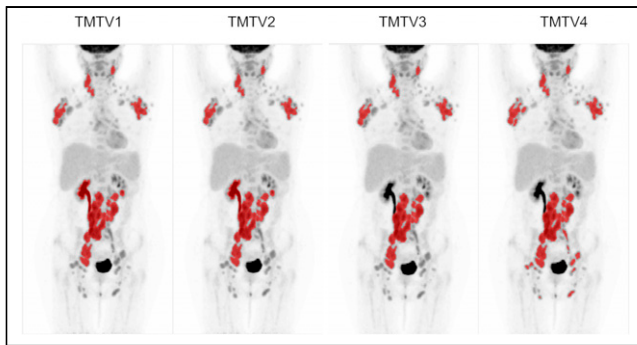


FIGURE 1. TMTVs for follicular lymphoma patient. TMTV3 shows removal of right renal uptake after manual editing, and TMTV4 included small lesions in pelvis and groin with SUV \geq 4.0 (volume $<$ 3 cm³) added using single mouse clicks.

Figure 2 illustrates the individually reported TMTVs against their reference values (median value among all readers for each patient), for TMTV1–TMTV4, and corresponding difference plots are given in Supplemental Figure 3. Excellent agreement was found between different readers with intraclass correlation coefficients greater than 0.96. There were no significant differences in any of the TMTVs or in any combination of readers ($P > 0.3$ in all cases). Figure 3 illustrates the TMTV obtained for the median TMTV2, TMTV3, and TMTV4 against the median reference TMTV1. In 70% of cases, TMTV4 equaled TMTV1 within 10 cm³. Figure 4 shows the final TMTV for individual readers against the final median reference TMTV from 3–4 readers. For the 8 cases with large discrepancies, the final TMTV results are provided in Table 1. For 5 of these 8 cases, large ($>$ 25%) differences were exclusively related to decisions about whether to include diffuse splenic uptake ($>$ 1.5 times liver uptake) (Fig. 5). The differences between TMTV4 and the other 3 cases ranged from approximately 50 cm³ to 100 cm³. The agreement between final TMTVs and the median value (per scan) was -10 ± 105 cm³ for all scans and 0.8 ± 22.5 cm³ after excluding the 5 patients with diffusely increased spleen uptake and 0.4 ± 10.5 cm³ after excluding patients listed in Table 1.

DISCUSSION

Baseline TMTV has emerged as an important prognostic factor in lymphoma subtypes (8,10,18). However, the lack of a standardized TMTV measurement procedure has been an important limitation for use in clinical trials and daily clinical practice. In Hodgkin lymphoma, for example, the reported TMTV cutoffs for optimal prognostication vary between 89 and 268 cm³ (23,37).

An international panel of experts was convened to develop an international benchmark for TMTV assessment of baseline ¹⁸F-FDG PET/CT in lymphoma patients. Considerations for the proposed workflow were that the method is widely available and easy to implement; has a high success rate in providing visually reasonable tumor outlines; is fast and easy to use, that is, with no or minimal manual corrections to generate segmentations; is little sensitive to variations in image quality or reconstruction settings; and demonstrates prognostic performance with a TMTV derived using the proposed method. The segmentation method using an SUV of at least 4.0 was selected as meeting these requirements (21,24,31). To minimize reader variability and to enhance segmentation speed, the workflow starts with automated preselection of lesions using an SUV of at least 4 and a volume of at least 3 cm³ and with a single-click removal of normal physiologic uptake. This workflow is available in the software tools in our study and, because of its simplicity, can be easily incorporated in any software.

With the proposed workflow, a final TMTV is obtained including all lesions with an SUV of at least 4 but with removal of high-uptake physiologic regions and manual edits of lesions close to or attached to high-physiologic-tissue regions, such as the brain, bladder, kidneys, and myocardium. These final baseline TMTVs were highly reproducible among multiple readers across 3 lymphoma subtypes, with differences in TMTV of less than 10 cm³ or 10% in 85% of the cases. Yet, in about 15% of cases, discrepancies in TMTV were caused by differences in manual editing of healthy tissues with high uptake (e.g., myocardium) or interpretation of diffuse splenic uptake. Hence, manual editing should be done carefully in complicated cases, although its impact on prognostic performance, when TMTV is combined with clinical characteristics, may be small (Supplemental File 6). Most cases with large

TABLE 1
Reported Final TMTVs for 8 Cases with Large Discrepancies in TMTV and Comments by Adjudicator About Causes

| Patient | TMTV (cm ³) | | | | Comments from adjudicator |
|---------|-------------------------|----------|----------|----------|---|
| | Reader 1 | Reader 2 | Reader 3 | Reader 4 | |
| H15 | 275 | 129 | 282 | — | Spleen |
| F02 | 426 | 399 | 456 | 252 | Spleen |
| F05 | 1,680 | 1,706 | 1,650 | 567 | Spleen |
| B10 | 786 | 788 | 49 | — | Spleen |
| B16 | 1,223 | 546 | 509 | — | Spleen |
| H11 | 178 | 229 | 137 | 159 | Physiologic uptake removed = 139 cm ³ ; manual addition of small multifocal uptake in BM, neck, and retroperitoneal increased to 231 cm ³ |
| B05 | 272 | 321 | 318 | — | Manual editing of myocardial uptake |
| F09 | 246 | 194 | 196 | 199 | Manual editing of kidneys and ureter |

H = Hodgkin lymphoma patient; — = missing data (some cases read by 3 readers only); F = follicular lymphoma patient; B = diffuse large B-cell lymphoma patient; BM = bone marrow.

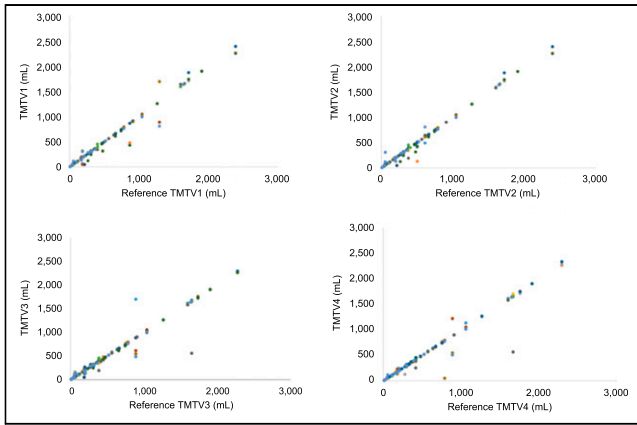


FIGURE 2. Individual reader TMTV measurements plotted against respective reference values. Different colors for symbols represent different readers.

discrepancies were explained by the interpretation of diffuse splenic uptake. In recent discussions among experts during the 9th International Workshop on PET in Lymphoma and Myeloma in Menton, France, in 2023, it was agreed that focal splenic uptake with an SUV greater than 4 should be included in the TMTV. However, the relevance of diffuse splenic uptake in prognostication was considered uncertain and was recognized to vary by lymphoma subtype, with diffuse reactive uptake in the spleen and bone marrow more commonly seen in Hodgkin lymphoma than in diffuse large B-cell lymphoma or follicular lymphoma (18). Consequently, in future studies, diffuse spleen uptake (and its volume) should be explored as a separate factor for determining prognosis.

Proposed Use of the Benchmark

The publicly available benchmark, consisting of PET/CT images, previews of the reported segmentations, TMTV4 segmentations, and reference TMTV values, can be used in several ways. First, for technical validation of new and existing clinical or research tools using the SUV4.0 method with minimum volume of 3 cm³ to evaluate if the local software can generate TMTVs that are similar (within 10% or 10 cm³) to the benchmark values as well as for clinical validation to evaluate if readers can generate comparable

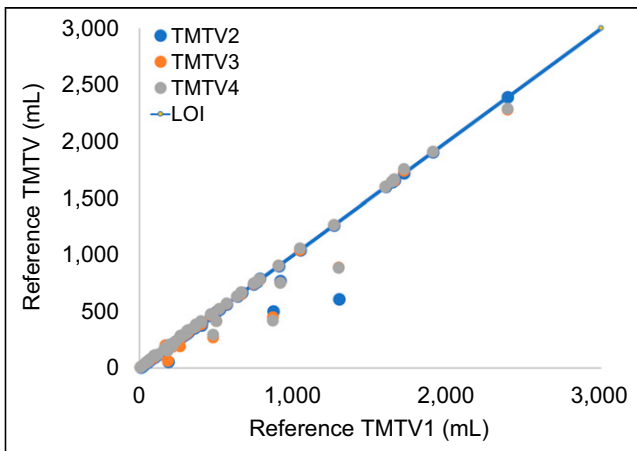


FIGURE 3. TMTV values for reference or median TMTV2, TMTV3, and TMTV4 against median initial preselection-based TMTV1. LOI = line of identity.

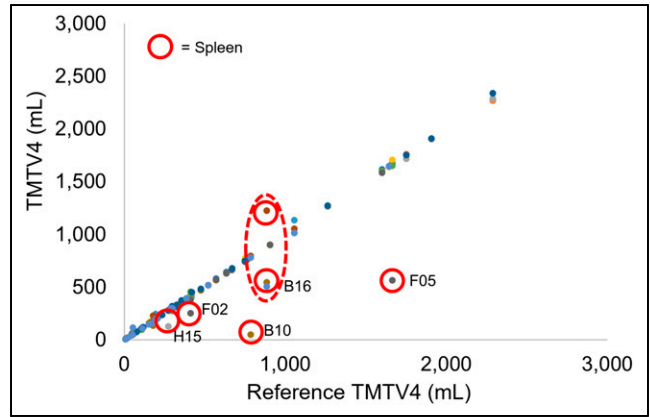


FIGURE 4. Correlation between TMTV4 assessed by 12 readers (in different colors) and median TMTV4 among readers per scan (reference). Close alignment with line of identity suggests excellent reader agreement. Outliers, indicated by red circles, were all related to interpretation of diffuse splenic uptake. Two outliers enclosed by dashed ellipse are from same scan of B-cell lymphoma patient 16 (B16) with 1 score above and 2 scores below median, in which readers disagreed whether to include spleen or not). For large outliers, patient IDs are indicated. B = diffuse large B-cell lymphoma patient; F = follicular lymphoma patient; H = Hodgkin lymphoma patient.

TMTVs (within 10% or 10 cm³) to international experts. Second, a locally validated benchmark workflow can be applied to new datasets and compared with novel segmentation methods to determine whether these provide improved clinical performance in datasets with available outcome data. Third, the benchmark can help remove the possible confounding effects of segmentation pipelines in multi-center studies or intersite comparisons, provided that each center reports compliance with the benchmark values. Possible examples of how to use the benchmark are given in Supplemental File 7.

Limitations

The scans were selected to cover the wide range of ¹⁸F-FDG uptake and distribution seen in lymphoma PET/CT studies and to provide experts with challenging TMTV measurement cases. Consequently, the cases are not necessarily representative of the true prevalence of disease distribution, including more cases with increased diffuse splenic uptake than usually seen in clinical practice. Yet, we

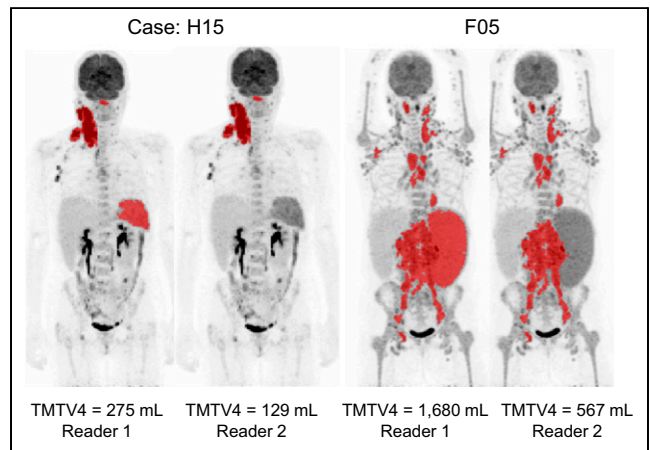


FIGURE 5. Maximum-intensity projections of Hodgkin lymphoma patient 15 (H15, left 2 panels) and follicular lymphoma patient 5 (F05, right 2 panels) with discrepant TMTV assessment between readers who chose to include or exclude spleen uptake. For other visible lesions, TMTVs were identical.

felt it was important to include these challenging patterns. The final dataset was approved by an international panel of experts, confirming that the dataset covers the complete range of ^{18}F -FDG uptake and distribution experienced in practice. It should be emphasized that the benchmark is not suitable (nor intended) for assessing the clinical performance of a segmentation method. On page 3 of Supplemental File 7, we explain how the benchmark could be used to clinically evaluate new segmentation methods.

Another limitation is that images were collected from existing retrospective clinical trials, and at the time of data collection, Evaluation and Report Language standards were neither fully established nor commonly applied. Because of the age of the datasets, images are likely comparable to the previous Evaluation and Report Language standard 1, although Evaluation and Report Language compliance cannot be stated or proven. However, this does not impact the applicability of the benchmark. The benchmark is intended to allow vendors, software developers, and users to validate their implementation of the benchmark tumor delineation method (SUV4.0) and to show that their tool can generate correct TMTVs by reporting the accuracy and precision of their measurements. The latter technical validation does not rely on the quality of the images used, as the reported benchmark TMTVs are based on these benchmark images. In this way, the benchmark can help to reduce variability in TMTV measurements due to differences in delineation methods or implementations.

This study was designed to provide a benchmark for baseline TMTV measurements, and the degree of uptake in most tumor lesions was higher, typically more than 2-fold, than liver uptake. The proposed segmentation method is unlikely to provide satisfactory TMTVs in interim or end-of-treatment scans, with lower uptake in smaller residual lesions. Other segmentation methods have been suggested for interim PET (38), and assessment of the optimal method for end-of-treatment scans is under evaluation. The SUV4.0 method will not always include all visible tumor regions or tumors. If and to what degree this affects TMTV as a prognostic or predictive factor is largely unexplored and is an intended use of the benchmark. By analyzing a clinical dataset, for example, of patients with classic Hodgkin lymphoma, using the benchmark method as well as any other method that includes low ^{18}F -FDG-avid regions or tumors, investigators can start to explore whether including these regions would result in better prognosis or predictions. Such a study was recently performed by Driessen et al. (22), who compared different tumor delineation methods and showed that, in the case of Hodgkin disease, TMTV based on the benchmark method still had the highest clinical prognostic performance among 6 common methods. The proposed benchmark aims at harmonizing TMTV measurements. However, other and better segmentation methods may exist or will be developed, with the expectation that new artificial intelligence-based approaches can provide TMTVs more quickly and reliably. The benchmark method should not be considered a gold standard but rather a universal reference method to test improvements in TMTV measurements or preferably its clinical value as a prognostic marker.

CONCLUSION

The proposed segmentation method and workflow allowed TMTVs to be generated with high reproducibility among readers and software tools, with minimal reader interaction in 70% of cases. The inclusion or exclusion of diffuse splenic uptake requires further study to define specific criteria that might vary according to lymphoma subtype. The TMTV dataset is publicly available as

a benchmark to allow imaging departments, software developers, and vendors to implement and validate the workflow. The proposed TMTV measurement workflow allows comparison, sharing, and pooling of study results. Moreover, it could serve as a reference to test potential improvements in the measurement of TMTV using other or artificial intelligence approaches. On the basis of our findings, we recommend that the SUV4.0 method should be included or at least tested in future clinical trials.

DISCLOSURE

Sally Barrington acknowledges support from the National Institute for Health and Care Research (NIHR) (RP-2016-07-001). This work was also supported by core funding from the Wellcome/EPSCRC Centre for Medical Engineering at King's College London (WT203148/Z/16/Z). The views expressed are those of the authors and not necessarily those of the NHS, the NIHR, or the Department of Health and Social Care. Heiko Schöder was supported in part by NIH/NCI Cancer Center Support Grant P30 CA008748. Ronald Boellaard is scientific advisor of the EARL PET/CT accreditation program. Salim Kanoun is the founder of the Pixilib imaging CRO. This work was carried out under the auspices of the International Workshops on PET in Lymphoma and Myeloma. Data were presented in part at the workshop on October 6, 2023, held in Menton, France. No other potential conflict of interest relevant to this work was reported.

ACKNOWLEDGMENTS

We thank Marc Andre, R. Olivier Casasnovas, Stefano Luminari, Franck Morschhauser, and John Raemaekers, who contributed the cases for the benchmark dataset, as principal investigators from the relevant clinical trials. We acknowledge the vision of our late colleague, Prof. Michel Meignan, founder of the international workshops on PET in lymphoma and myeloma (<https://www.lymphomapet.com/>), whose leadership inspired the development of MTV as a biomarker.

KEY POINTS

QUESTION: Can we measure TMTV in ^{18}F -FDG PET/CT studies of lymphoma patients in a reliable and reproducible manner?

PERTINENT FINDINGS: TMTV was measured reliably and reproducibly in 60 lymphoma cases from clinical trials by 12 international experts using a standardized segmentation method and workflow with freely available academic software. TMTV was easily measured in most cases with minimal reader interaction. The images and segmentations are provided as a benchmark dataset for PET readers, software developers, and vendors to estimate their ability to measure TMTV consistently with expected values. The benchmark can be used for comparison of the technical and clinical performance of other new segmentation methods.

IMPLICATIONS FOR PATIENT CARE: TMTV is an established prognostic factor in lymphoma. Our proposed benchmark provides a standardized and practical measurement method for TMTV to facilitate its use as a reliable biomarker in patient care and clinical research.

REFERENCES

1. Barrington SF, Trotman J. The role of PET in the first-line treatment of the most common subtypes of non-Hodgkin lymphoma. *Lancet Haematol*. 2021;8:e80–e93.

2. Cottreau AS, Versari A, Loft A, et al. Prognostic value of baseline metabolic tumor volume in early-stage Hodgkin lymphoma in the standard arm of the H10 trial. *Blood*. 2018;131:1456–1463.
3. Luminari S, Manni M, Galimberti S, et al. Response-adapted postinduction strategy in patients with advanced-stage follicular lymphoma: the FOLL12 study. *J Clin Oncol*. 2022;40:729–739.
4. Trotman J, Barrington SF. The role of PET in first-line treatment of Hodgkin lymphoma. *Lancet Haematol*. 2021;8:e67–e79.
5. El-Galaly TC, Villa D, Gormsen LC, Baech J, Lo A, Cheah CY. FDG-PET/CT in the management of lymphomas: current status and future directions. *J Intern Med*. 2018;284:358–376.
6. Cottreau AS, Rebaud L, Trotman J, et al. Metabolic tumor volume predicts outcome in patients with advanced stage follicular lymphoma from the RELEVANCE trial. *Ann Oncol*. 2024;35:130–137.
7. Cottreau AS, Meignan M, Nioche C, et al. Risk stratification in diffuse large B-cell lymphoma using lesion dissemination and metabolic tumor burden calculated from baseline PET/CT. *Ann Oncol*. 2021;32:404–411.
8. Eertink JJ, Zwezerijnen GJC, Heymans MW, et al. Baseline PET radiomics outperforms the IPI risk score for prediction of outcome in diffuse large B-cell lymphoma. *Blood*. 2023;141:3055–3064.
9. Meignan M, Cottreau AS, Versari A, et al. Baseline metabolic tumor volume predicts outcome in high-tumor-burden follicular lymphoma: a pooled analysis of three multicenter studies. *J Clin Oncol*. 2016;34:3618–3626.
10. Mikhaeel NG, Heymans MW, Eertink JJ, et al. Proposed new dynamic prognostic index for diffuse large B-cell lymphoma: international metabolic prognostic index. *J Clin Oncol*. 2022;40:2352–2360.
11. Thieblemont C, Chartier L, Duhsen U, et al. A tumor volume and performance status model to predict outcome before treatment in diffuse large B-cell lymphoma. *Blood Adv*. 2022;6:5995–6004.
12. Mikhaeel NG, Smith D, Dunn JT, et al. Combination of baseline metabolic tumour volume and early response on PET/CT improves progression-free survival prediction in DLBCL. *Eur J Nucl Med Mol Imaging*. 2016;43:1209–1219.
13. Allen PB, Lu X, Chen Q, et al. Sequential pembrolizumab and AVD are highly effective at any PD-L1 expression level in untreated Hodgkin lymphoma. *Blood Adv*. 2023;7:2670–2676.
14. Voltin CA, Mettler J, van Heek L, et al. Early response to first-line anti-PD-1 treatment in Hodgkin lymphoma: a PET-based analysis from the prospective, randomized phase II NIVAHL trial. *Clin Cancer Res*. 2021;27:402–407.
15. Cottreau AS, Buvat I, Kanoun S, et al. Is there an optimal method for measuring baseline metabolic tumor volume in diffuse large B cell lymphoma? *Eur J Nucl Med Mol Imaging*. 2018;45:1463–1464.
16. Cottreau AS, Hapdey S, Chartier L, et al. Baseline total metabolic tumor volume measured with fixed or different adaptive thresholding methods equally predicts outcome in peripheral T cell lymphoma. *J Nucl Med*. 2017;58:276–281.
17. Ilyas H, Mikhaeel NG, Dunn JT, et al. Defining the optimal method for measuring baseline metabolic tumour volume in diffuse large B cell lymphoma. *Eur J Nucl Med Mol Imaging*. 2018;45:1142–1154.
18. Barrington SF, Meignan M. Time to prepare for risk adaptation in lymphoma by standardizing measurement of metabolic tumor burden. *J Nucl Med*. 2019;60:1096–1102.
19. Revailler W, Cottreau AS, Rossi C, et al. Deep learning approach to automatize TMTV calculations regardless of segmentation methodology for major FDG-avid lymphomas. *Diagnostics (Basel)*. 2022;12:417.
20. Kanoun S, Tal I, Berriolo-Riedinger A, et al. Influence of software tool and methodological aspects of total metabolic tumor volume calculation on baseline [¹⁸F]FDG PET to predict survival in Hodgkin lymphoma. *PLoS One*. 2015;10:e0140830.
21. Barrington SF, Zwezerijnen B, de Vet HCW, et al. Automated segmentation of baseline metabolic total tumor burden in diffuse large B-cell lymphoma: which method is most successful—a study on behalf of the PETRA consortium. *J Nucl Med*. 2021;62:332–337.
22. Driessen J, Zwezerijnen GJC, Schoder H, et al. The impact of semiautomatic segmentation methods on metabolic tumor volume, intensity, and dissemination radiomics in ¹⁸F-FDG PET scans of patients with classical Hodgkin lymphoma. *J Nucl Med*. 2022;63:1424–1430.
23. El-Galaly TC, Villa D, Cheah CY, Gormsen LC. Pre-treatment total metabolic tumour volumes in lymphoma: does quantity matter? *Br J Haematol*. 2022;197:139–155.
24. Ferrández MC, Eertink JJ, Golla SSV, et al. Combatting the effect of image reconstruction settings on lymphoma [¹⁸F]FDG PET metabolic tumor volume assessment using various segmentation methods. *EJNMMI Res*. 2022;12:44.
25. André MPE, Girinsky T, Federico M, et al. Early positron emission tomography response-adapted treatment in stage I and II Hodgkin lymphoma: final results of the randomized EORTC/LYSA/FIL H10 trial. *J Clin Oncol*. 2017;35:1786–1794.
26. Casasnovas RO, Bouabdallah R, Brice P, et al. PET-adapted treatment for newly diagnosed advanced Hodgkin lymphoma (AHL2011): a randomised, multicentre, non-inferiority, phase 3 study. *Lancet Oncol*. 2019;20:202–215.
27. Casasnovas RO, Ysebaert L, Thieblemont C, et al. FDG-PET-driven consolidation strategy in diffuse large B-cell lymphoma: final results of a randomized phase 2 study. *Blood*. 2017;130:1315–1326.
28. Morschhauser F, Fowler NH, Feugier P, et al. Rituximab plus lenalidomide in advanced untreated follicular lymphoma. *N Engl J Med*. 2018;379:934–947.
29. Nioche C, Orhac F, Boughdad S, et al. LIFEx: a freeware for radiomic feature calculation in multimodality imaging to accelerate advances in the characterization of tumor heterogeneity. *Cancer Res*. 2018;78:4786–4789.
30. Schindelin J, Arganda-Carreras I, Frise E, et al. Fiji: an open-source platform for biological-image analysis. *Nat Methods*. 2012;9:676–682.
31. Burggraaff CN, Rahman F, Kassner I, et al. Optimizing workflows for fast and reliable metabolic tumor volume measurements in diffuse large B cell lymphoma. *Mol Imaging Biol*. 2020;22:1102–1110.
32. Voltin C-A, Goergen H, Baues C, et al. Value of bone marrow biopsy in Hodgkin lymphoma patients staged by FDG PET: results from the German Hodgkin Study Group trials HD16, HD17, and HD18. *Ann Oncol*. 2018;29:1926–1931.
33. Barrington SF, Kirkwood AA, Franceschetto A, et al. PET-CT for staging and early response: results from the response-adapted therapy in advanced Hodgkin lymphoma study. *Blood*. 2016;127:1531–1538.
34. El-Galaly TC, d'Amore F, Mylam KJ, et al. Routine bone marrow biopsy has little or no therapeutic consequence for positron emission tomography/computed tomography-staged treatment-naïve patients with Hodgkin lymphoma. *J Clin Oncol*. 2012;30:4508–4514.
35. Cerci JJ, Györke T, Fanti S, et al. Combined PET and biopsy evidence of marrow involvement improves prognostic prediction in diffuse large B-cell lymphoma. *J Nucl Med*. 2014;55:1591–1597.
36. Luminari S, Biasoli I, Arcaini L, et al. The use of FDG-PET in the initial staging of 142 patients with follicular lymphoma: a retrospective study from the FOLL05 randomized trial of the Fondazione Italiana Linfomi. *Ann Oncol*. 2013;24:2108–2112.
37. Barrington SF. Advances in positron emission tomography and radiomics. *Hematol Oncol*. 2023;41(suppl 1):11–19.
38. Zwezerijnen GJC, Eertink JJ, Burggraaff CN, et al. Interobserver agreement on automated metabolic tumor volume measurements of Deauville score 4 and 5 lesions at interim ¹⁸F-FDG PET in diffuse large B-cell lymphoma. *J Nucl Med*. 2021;62:1531–1536.