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RESEARCH

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Reliability of the nitrogen washin-washout technique to assess end-expiratory lung volume at variable PEEP and tidal volumes

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Abstract

Background: End-expiratory lung volume measurement by the nitrogen washin-washout technique (EELV_{WI-WO}) may help titrating positive end-expiratory pressure (PEEP) during acute respiratory distress syndrome (ARDS). Validation of this technique has been previously performed using computed tomography (EELV_{CT}), but at mild PEEP levels, and relatively low fraction of inspired oxygen (FiO₂), which may have insufficiently challenged the validity of this technique. The aims of this study were (1) to evaluate the reliability of EELV_{WI-WO} measurements at different PEEP and V_T during experimental ARDS and (2) to evaluate trending ability of EELV_{WI-WO} to detect EELV changes over time.

Methods: ARDS was induced in 14 piglets by saline lavage. Optimal PEEP was selected during a decremental PEEP trial, based on best compliance, best EELV_{WI-WO}, or a PEEP-FiO₂ table. Eight V_T (4 to 20 mL · kg⁻¹) were finally applied at optimal PEEP. EELV_{WI-WO} and EELV_{CT} were determined after ARDS onset, at variable PEEP and V_T.

Results: EELV_{WI-WO} underestimated EELV_{CT} with a non-constant linear bias, as it decreased with increasing EELV. Limits of agreement for bias were ±398 mL. Bias between methods was greater at high PEEP, and further increased when high PEEP was combined with low V_T. Concordance rate of EELV changes between consecutive measurements was fair (79%). Diagnostic accuracy was good for detection of absolute EELV changes above 200 mL (AUC = 0.79).

Conclusions: The reliability of the WI-WO technique is critically dependent on ventilatory settings, but sufficient to accurately detect EELV change greater than 200 mL.

Keywords: ARDS; End-expiratory lung volume; Computed tomography; PEEP

Background

Acute respiratory distress syndrome (ARDS) is characterized by a major decrease in lung aerated volume. End-expiratory lung volume measurement by the nitrogen washin-washout technique (EELV_{WI-WO}) [1] is available at the bedside from an ICU ventilator, and may help titrating PEEP during mechanical ventilation of ARDS patients. Validation of this technique has been previously performed in mechanically ventilated patients using computed tomography (CT) as gold standard [2], but at relatively low PEEP levels (5 cm H₂O), low fraction of inspired oxygen (FiO₂) and respiratory

rate (RR), and with tidal volume (V_T) $8 \pm 1 \text{ mL} \cdot \text{kg}^{-1}$ in the upper range of current experts' recommendations for ARDS management [3]. Such ventilatory settings may have insufficiently challenged the validity of this technique, which requires a constant inhomogeneity in alveolar gas throughout the measurement, and may be less precise at FiO_2 greater than 0.7 [1].

Furthermore, the WI-WO technique is particularly suitable for repeated EELV assessment, and hence to identify EELV trends, but has never been formally validated for this purpose.

The aims of this study were to evaluate (1) the reliability of $\text{EELV}_{\text{WI-WO}}$ measurement at variable PEEP and V_T , at high RR and FiO_2 during experimental ARDS, using CT as a reference and (2) the trending ability of WI-WO technique to detect change in EELV associated with PEEP and V_T variations.

Methods

This study was approved by our Institutional Review Board for the care of animal subjects (Comité d'expérimentation animale de l'université Lyon I), and carried out in 14 pigs ($28 \pm 2 \text{ kg}$).

Animal preparation

Pigs were anesthetized with propofol and fentanyl, tracheotomized and mechanically ventilated in volume-controlled mode, with constant inspiratory flow, V_T $10 \text{ mL} \cdot \text{kg}^{-1}$, inspired fraction of oxygen (FiO_2) 0.21, zero end-expiratory pressure, and RR adjusted to achieve normocapnia using Engström Carestation® ventilator (General Electric Healthcare, Madison, WI, USA). Muscle relaxation was obtained with pancuronium bromide. Right jugular vein was cannulated with a 3-lumen 8.5-Fr catheter for drug administration. Carotid artery was cannulated with an 8.5 Fr catheter. FiO_2 was increased to 1 at the end of animal preparation.

Measurements

Air flow was measured using a small volume pneumotachograph (PN 281637, Hamilton medical AG, Bonaduz, Switzerland). Pressure at the airway opening was measured using a connecting tube with lateral aperture connected between the endotracheal tube and the pneumotachograph. Signals of arterial blood pressure, pressure at the airway opening, and air flow were read by transducers (Becton Dickinson, Sandy, UT, USA), connected to an A/D card (MP 100; Biopac Systems, Santa Barbara, CA, USA), acquired at 200 Hz and analyzed with Acknowledge® software (Biopac Systems, Santa Barbara, CA, USA). Tracheal pressure was measured through an air filled catheter introduced down the endotracheal tube, positioned 2 cm distal to the tube tip, and connected to the ventilator, to obtain alveolar pressure [4].

$\text{EELV}_{\text{WI-WO}}$ was assessed by the ventilator, by using the nitrogen washout/washin technique [1], from continuous measurement of end-tidal O_2 and CO_2 during a 0.1 change of FiO_2 using pediatric sensors (Pedi-lite+, Dahtex-Ohmeda Inc, Madison, WI, USA). The average value of the washout and washin measurements during 1 to 0.9 and 0.9 to 1 FiO_2 changes was given by the ventilator.

EELV_{CT} was calculated using lung CT, as previously described [2]. CT calibration using the manufacturer phantom was performed before each CT study. The CT scanner (Biograph mCT/S, Siemens, Munich, Germany) was set as follows: interval 1 mm, voltage 120 kV, pitch 1.2 mm, and field of view 300 mm. Whole lung CT images were taken during 15 s end-expiratory. CT raw data were reconstructed as 1-mm-thick contiguous slices using a medium smooth filter (B31f). Image segmentation was manually performed over the whole lung using Turtleseg® software [5,6] (www.turtleseg.org). Gas volume in each lung voxel was computed from the CT number using the following formulas [2]:

$$\text{Gas volume} = \left(\frac{\text{CTnumber}}{-1,000} \right) \times \text{voxel volume for lung voxels with CT number} \leq 0.$$

Gas volume = 0 for lung voxels with CT number > 0.

EELV_{CT} was computed as the sum of gas volume in all the voxels defined by lung segmentation.

Expected EELV on zero end-expiratory pressure was deemed as 33 mL · kg⁻¹ body weight as previously published in normal anesthetized pigs [7].

Protocol

ARDS was performed by saline lavage at ventilatory settings mentioned above. Intra-tracheal instillations of 1,000 mL aliquots of 0.9% sodium chloride warmed at 37°C were repeated until PaO₂/FiO₂ ratio was <100 mmHg. RR may be increased up to 35 breaths per min to maintain pH above 7.20, then kept constant except at the end of experiment, where at the highest V_T, it was decreased to maintain peak airway pressure below 100 cm H₂O.

Then, PEEP was set to 20 cm H₂O, V_T to 6 mL · kg⁻¹, and a recruitment maneuver was performed by applying a continuous airway pressure of 40 cm of H₂O over 40 s. A decremental PEEP trial was then performed from 20 to 2 cm H₂O by 2 cm H₂O steps of 10 min each. At the end of the decremental PEEP trial, animals were randomized into three PEEP groups, for which PEEP level was set according to either highest compliance (*n* = 4), or highest EELV_{WI-WO} (*n* = 5), or PEEP-FiO₂ table (*n* = 4) [8]. This randomization was used to deliver a wide PEEP range during the final part of the study, in order to obtain multiple combinations of PEEP and V_T, so as to perform a multivariate analysis adjusted for PEEP and V_T. One pig died just after the PEEP trial before randomization, and was kept in the final analysis. The selected PEEP was applied for 1 h, and V_T was adjusted to maintain plateau pressure of the respiratory system ≤30 cm of H₂O.

After 1 h of applied selected PEEP, eight levels of V_T (4, 5, 6, 7, 8, 10, 15, 20 mL · kg⁻¹) ranging from 100 to 625 mL, were applied for 2 min leaving PEEP level unchanged. EELV_{WI-WO} and EELV_{CT} were measured immediately after ARDS onset, at the end of each PEEP step during the PEEP trial, and at the end of each V_T change. A 15-s end-inspiratory pause was performed to check the absence of air leak in each experimental condition. Some experimental conditions were not available since pneumothorax occurred in several pigs at high V_T or since EELV_{WI-WO} values were lacking for technical reasons, ending up in 218 data points in final analysis (see Additional file 1: Table S1 for description of lacking data points).

Statistical analysis

Statistical analyses were performed using R software [9], with packages nlme [10], MethComp [11], pROC [12], OptimalCutpoints [13], and multcomp [14]. Values were expressed as mean \pm standard deviation (SD). The level of statistical significance was set below 0.05.

EELV_{WI-WO} and EELV_{CT} were compared using a linear mixed-effects model, and Bland and Altman representation [15]. Limits of agreement were computed using alternating regression [16] since bias was non-constant and the experimental design involved repeated measurements.

To control for an effect of confounding variables on the bias, a linear mixed-effects model was built using PEEP, V_T , EELV_{CT} at ARDS onset and their interactions as factors with fixed effect, pigs as factor with random effect [17], and bias as dependent variable. Model simplification was performed using a backward stepwise algorithm.

Percentage error was computed as $\times SD_{\text{Bias}}/\text{mean}_{\text{EELV}}$ [18]. As percentage error was not reported in the two previously published studies that compared EELV_{WI-WO} and EELV_{CT} [2,19], Cartesian data of these studies were reanalyzed, being uplifted using a scientific program allowing extraction of individual data points from a digitalized graph (DataThief III[®] [20]) as follows: a digital copy of each regression plot was analyzed with DataThief from the portable document format file of the journal articles, and the extracted data were exported as two columns of X-Y coordinates, with each row representing an extracted data point, allowing computation of percentage error of each study.

Changes in EELV between consecutive measurements were computed for EELV_{WI-WO} ($\Delta\text{EELV}_{\text{WI-WO}}$) and EELV_{CT} ($\Delta\text{EELV}_{\text{CT}}$). Ability of the WI-WO technique to track changes in EELV was assessed using four-quadrant and polar plots. The four-quadrant plot relates $\Delta\text{EELV}_{\text{WI-WO}}$ and $\Delta\text{EELV}_{\text{CT}}$, with upper right and lower left quadrants being quadrants of agreement (in which both EELV_{WI-WO} and EELV_{CT} have the same directional changes) and lower right and upper left quadrants being quadrants of disagreement (in which EELV_{WI-WO} and EELV_{CT} have opposite directional changes). Concordance rate was defined as the percentage of data points falling into one of the two quadrants of agreement, expressed as a percentage of the total number of data points [21]. The main drawback of the four-quadrant plot is the lack of quantification of the distance between each data point and the line of identity, leading to the development of polar plot analysis [21]. Polar plot is obtained by a 45° clockwise rotation of the four-quadrant plot, changing the dimensions of the radius to mean ΔEELV [22], lining up the line of identity along the horizontal axis. Data points with positive and negative directional changes are located on the right and the left side of the polar plot, respectively, and the polar angle represents the angle of each data point with line of identity. A 0° polar angle depicts a perfect agreement between $\Delta\text{EELV}_{\text{WI-WO}}$ and $\Delta\text{EELV}_{\text{CT}}$, while polar angles in the range 45° to 135° and 225° to 315° depict disagreement between directional changes of EELV_{WI-WO} and EELV_{CT}. The following variables are computed from polar plots: (1) angular bias as the mean angle between all data points and polar axis [21], reflects the difference in calibration between the reference and test methods; (2) radial limits of agreement as the radial sector containing 95% of the data points, after conversion of negative deflections to positive ones, is a polar version of the 95% confidence limits and is similar to the limits of agreement in Bland and Altman analysis [21].

Bias and angular bias were compared to zero using Mann-Whitney *U* test. Multiple comparisons were performed with Dunnett's test using PEEP 0 as a reference.

The ability of the WI-WO technique to detect a change in EELV greater than 100, 150, 200, 250, and 300 mL was tested by computations of area under receiver operating characteristic (AUC) curve. The optimal cut-off points were computed using the Youden J statistic.

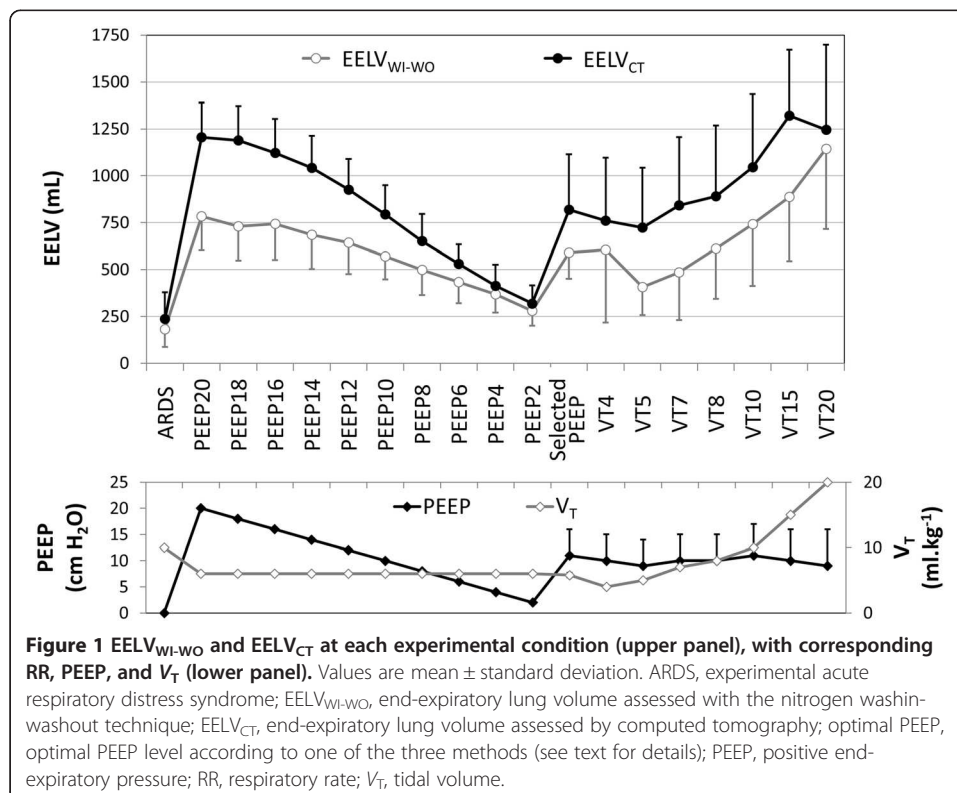
Results

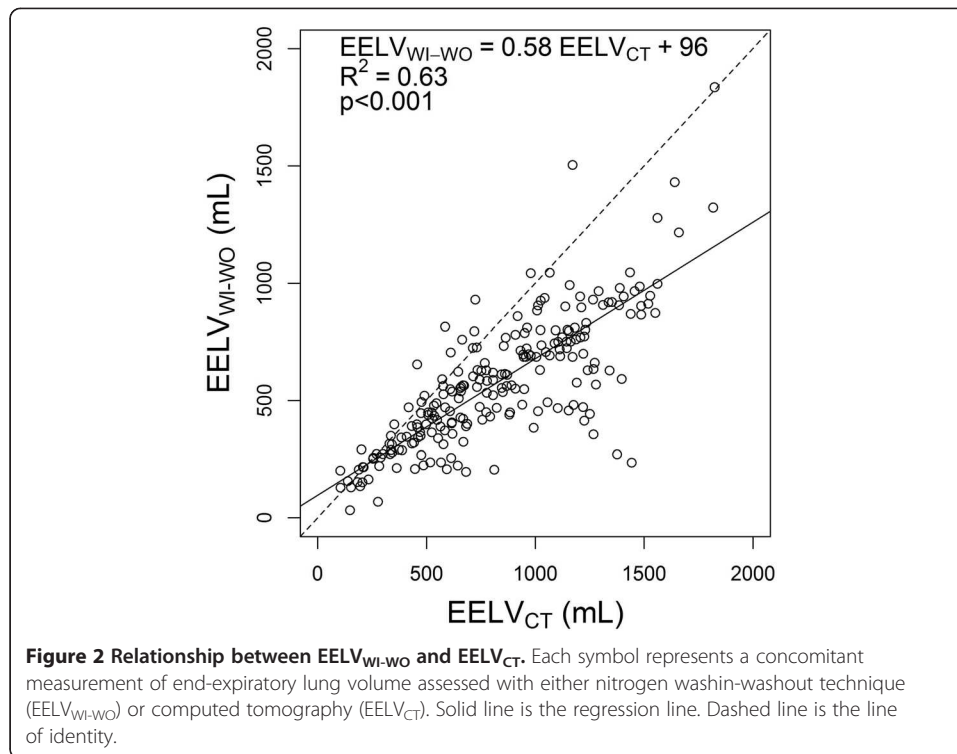
Ventilatory settings and arterial blood gases during the whole experiment are reported in Additional file 2: Table S2. Figure 1 depicts the evolution of $EELV_{WI-WO}$ and $EELV_{CT}$ over time. Immediately after ARDS onset, $EELV_{CT}$ was very low (236 ± 143 mL (25% \pm 15% of its theoretical value, range 104 to 668 mL)), and increased to $1,206 \pm 185$ mL (range 957 to 1,528 mL) at PEEP 20.

$EELV_{CT}$ and $EELV_{WI-WO}$ values were very close at PEEP 0, but their difference progressively increased with the PEEP level.

Comparison of $EELV_{WI-WO}$ and $EELV_{CT}$

$EELV_{WI-WO}$ and $EELV_{CT}$ were significantly correlated ($R^2 = 0.63$, $p < 0.001$). The regression equation between $EELV_{WI-WO}$ and $EELV_{CT}$, had an intercept of 96 mL ($p < 0.001$) and a slope of 0.58 mL^{-1} ($p < 0.001$; Figure 2). Bland and Altman representation exhibited a non-constant bias, decreasing toward more negative values as mean EELV





increased (Figure 3). The difference between EELV_{WI-WO} and EELV_{CT} was related to their mean value by the following equation:

$$EELV_{WI-WO} - EELV_{CT} = -1.28 - 0.33 \times (EELV_{WI-WO} + EELV_{CT}) / 2. \quad (1)$$

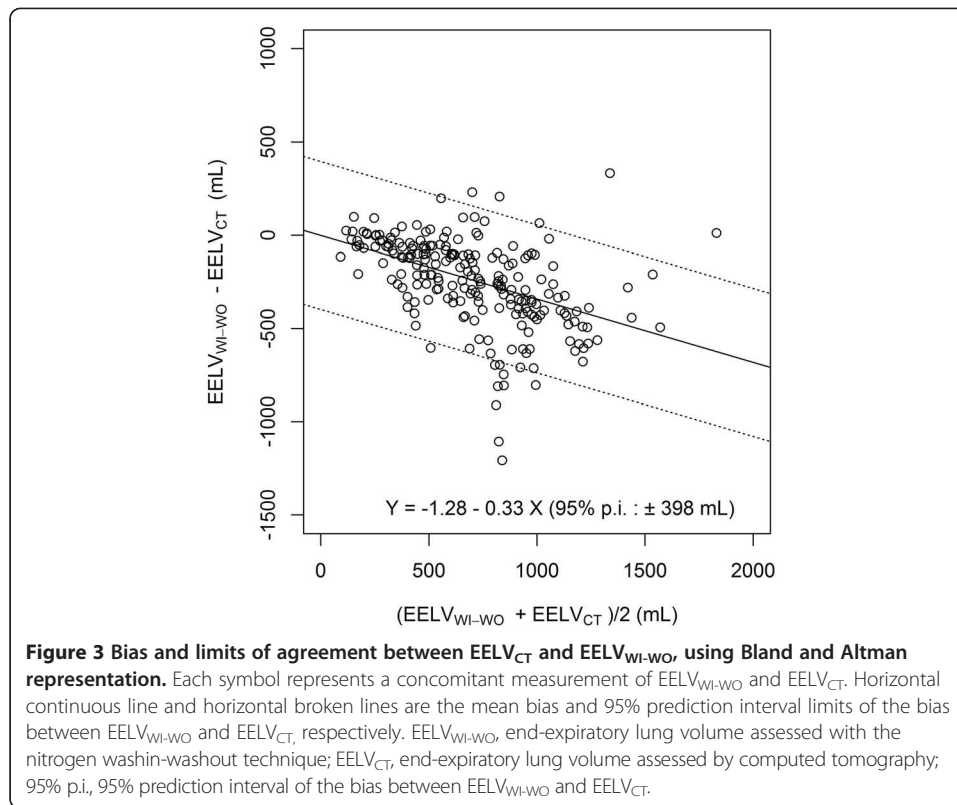
Limits of agreement of the bias were ± 398 mL (Figure 3), and percentage error was computed to 57%. A significant interaction between PEEP, V_T , EELV baseline value on the bias between methods was identified (Table 1) and reported (Figure 4). The bias between methods was strongly influenced by PEEP level, increasing at higher PEEP regardless the V_T level. The bias further increased when high PEEP was combined to low V_T , when EELV at baseline was low.

The bias at PEEP 0 amounted to -54 ± 101 mL, was not significantly different from 0, and was compared to bias values at higher PEEP. As shown in Figure 5, the bias at PEEP 10 and higher did significantly differ from PEEP 0, while non-significant differences were found for lower PEEP.

Assessment of trending ability of the WI-WO technique

$\Delta EELV_{WI-WO}$ values adequately tracked $\Delta EELV_{CT}$ changes against time (Figure 6). Concordance rate over all measurements amounted to 79%, and slightly increased after exclusion of small changes in EELV which do not reflect trending ability (Table 2).

Results of the polar plot analysis are reported in Figure 7, and in Table 2. The angular bias amounted to $-4^\circ \pm 37^\circ$ for all measurements. After exclusion of EELV changes ≤ 100 mL, the angular bias amounted to $3^\circ \pm 25^\circ$, and was not statistically different from 0. Radial limits of agreement were wide when all measurements were taken into account ($\pm 78^\circ$), but were narrowed to $\pm 51^\circ$ after exclusion of EELV

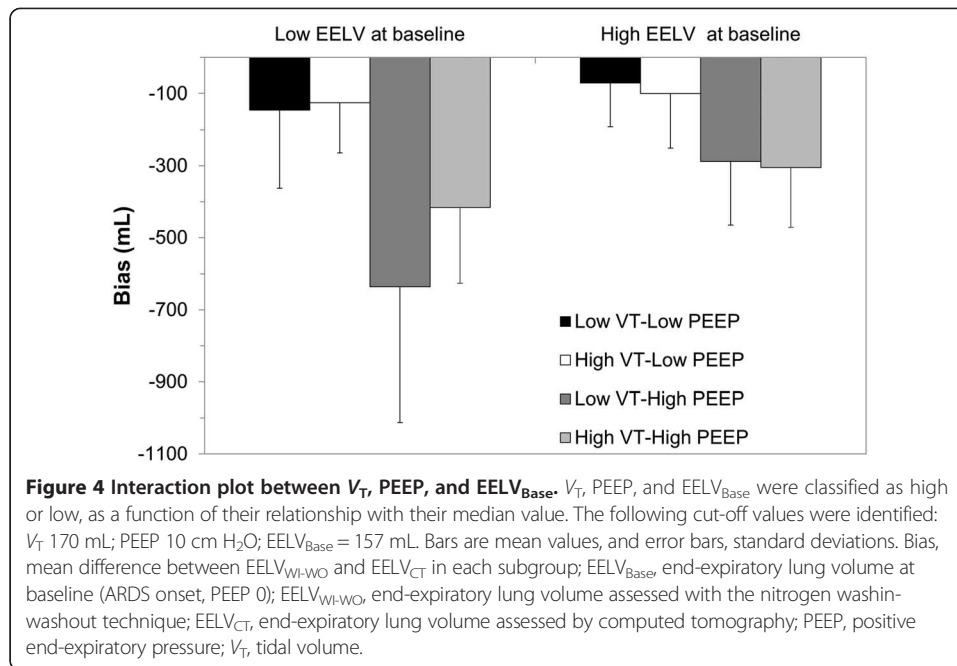


changes ≤ 100 mL. Increasing the exclusion threshold of EELV changes up to 300 mL did not improve the radial limits of agreement (Table 2). Diagnostic performance of EELV_{WI-WO} to detect absolute EELV changes greater than 100, 150, 200, 250, and 300 mL is presented in Table 3. Diagnosis accuracy was fair for detection of absolute EELV changes above 200 mL (AUC 0.79 (CI 95% 0.70 to 0.89)), and good for detection of absolute EELV changes above 300 mL (AUC 0.89 (CI 95% 0.83 to 0.95)).

Table 1 Statistical modeling of the bias between EELV_{WI-WO} and EELV_{CT} as a function of confounding variables

	AIC	Statistical significance
Model 1: No explanatory variable	2992	
Model 2: Adjusting for V_T	2994	$V_T: p = 0.55$
Model 3: Adjusting for PEEP	2868	PEEP: $p < 0.0001$
Model 4: Adjusting for EELV _{Base}	2980	EELV _{Base} : $p < 0.0001$
Model 5: Final model adjusting for V_T , PEEP, EELV _{Base} and their three-way interaction	2821	three-way interaction: $p < 0.0001$ $V_T \times$ PEEP interaction: $p < 0.0001$ $V_T \times$ EELV _{Base} : $p < 0.001$ PEEP \times EELV _{Base} : $p < 0.0001$ $V_T: p < 0.001$ PEEP: $p < 0.0001$ EELV _{Base} : $p < 0.05$

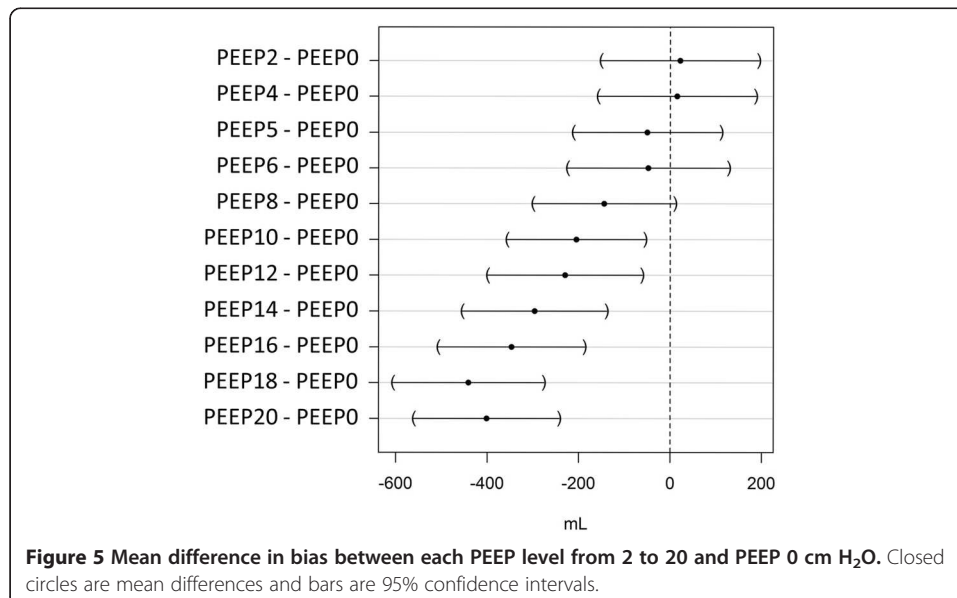
AIC, Akaike information criterion; EELV, end-expiratory lung volume; EELV_{Base}, EELV baseline value (ARDS onset, PEEP 0 cm H₂O); PEEP, positive end-expiratory pressure; V_T , tidal volume.

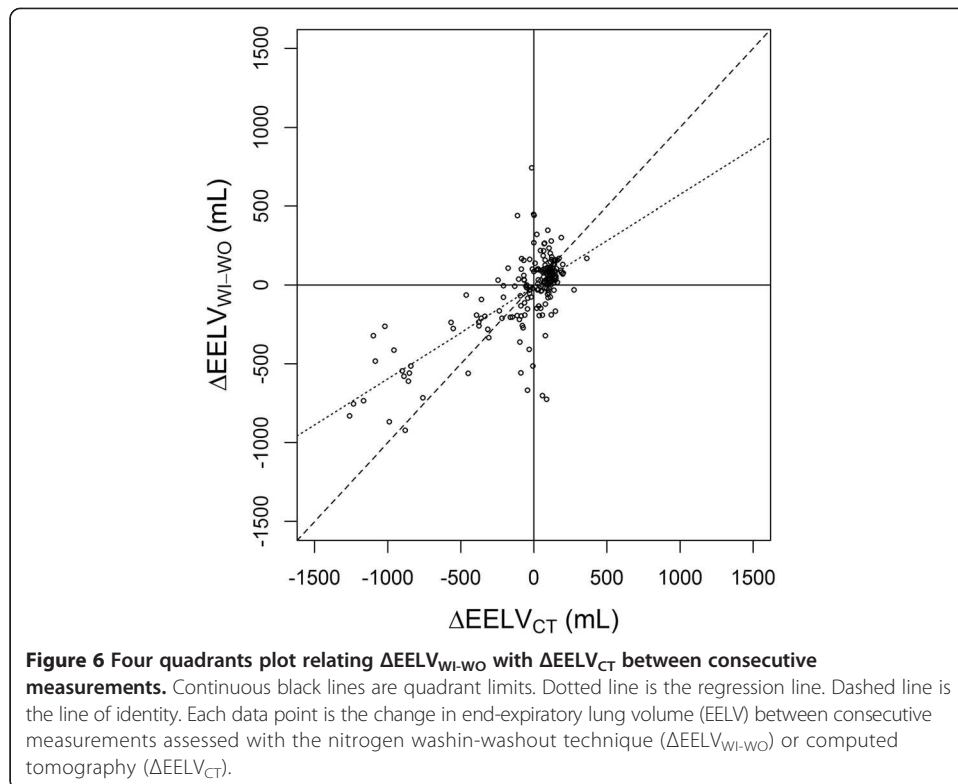


Discussion

The main findings of the present study are that, in experimental ARDS, (1) $EELV_{WI-WO}$ underestimates $EELV_{CT}$, and this underestimation increases linearly as $EELV$ increases; (2) this underestimation is dependent on ventilatory settings (mainly PEEP); (3) the precision of this technique is poor with a percentage error as high as 57%; (4) this technique is however reliable to detect an $EELV$ change greater than 200 mL.

A formal comparison between $EELV_{WI-WO}$ and $EELV_{CT}$ has already been performed in a pig model of pleural effusion [19] and in mechanically ventilated patients [2]. While Chiumello et al. found a slightly positive constant bias between $EELV_{WI-WO}$ and $EELV_{CT}$ [2], and Graf et al. a slightly negative constant bias, a non-constant linear bias





was found in the present study. Beside differences in species, experimental protocol or mechanism of lung injury, the likely explanation of this discrepancy is related to the higher PEEP level applied in the present study (up to 20 cm H₂O), while PEEP was set to 5 cm H₂O in the human study [2] and ≤ 10 cm H₂O in the animal study [19]. The dependence of bias on PEEP level was further emphasized in our study by multivariate analysis (Table 1, Figure 4), more specifically for PEEP levels greater than 10 cm H₂O. Finally, a detrimental effect of PEEP levels greater than 16 cm H₂O on EELV_{WI-WO} accuracy was also recently pointed out by Dellamonica et al. [23]. Nevertheless, in spite of a non-constant bias, the true EELV value may still be assessed by the WI-WO technique using Equation 1, as pointed out by Bland and Altman [24].

The detrimental effect of high PEEP levels on the bias may have multiple explanations. First, the WI-WO technique measures volume of lung regions that may be reached by nitrogen (and hence are ventilated), while CT measures aeration of both ventilated and non-ventilated regions. One could then hypothesize that regional ventilation (and hence nitrogen during EELV measurement) at high PEEP may be

Table 2 Concordance rate, angular bias, and radial limits of agreement in different data subsets

	No exclusion zone	Exclusion threshold 100 mL	Exclusion threshold 150 mL	Exclusion threshold 200 mL	Exclusion threshold 300 mL
Concordance rate	79%	82%	82%	86%	86%
Angular bias \pm SD (°)	-4 ± 37	3 ± 25	6 ± 25	1 ± 26	-1 ± 25
Radial limits of agreement (°)	± 78	± 51	± 48	± 48	± 50

Exclusion threshold refers to exclusion of data points with change in end-expiratory lung volume between consecutive time points below or equal to 100, 150, 200, and 300 mL, respectively. *SD*, standard deviation.

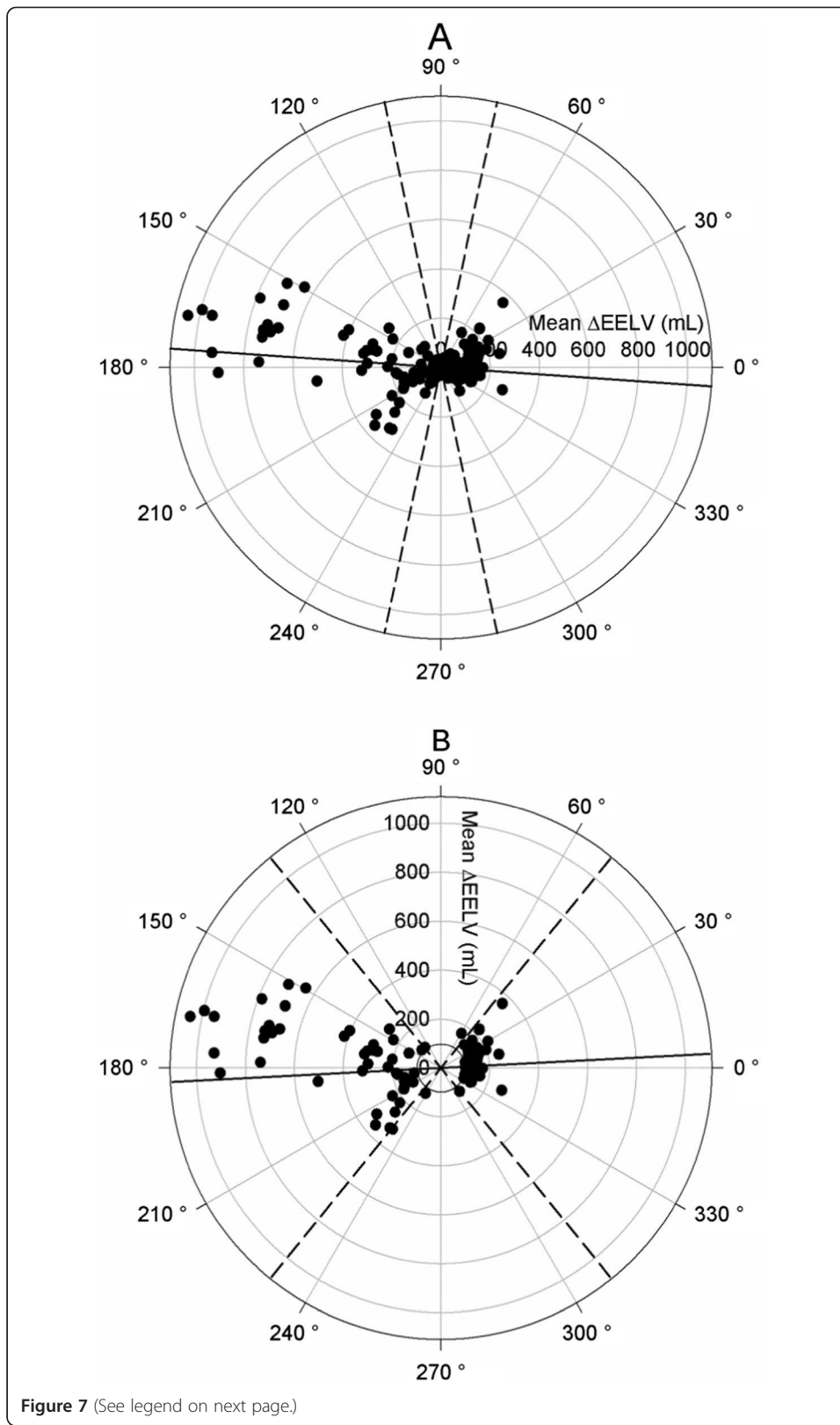


Figure 7 (See legend on next page.)

(See figure on previous page.)

Figure 7 Polar plots assessing trending ability of EELV_{WI-WO} to track changes in EELV. Panel A refers to the whole set of measurements, and panel B is restricted to data related to changes in EELV greater than 100 mL since a small change in EELV does not reflect trending ability but mainly random error measurement. The radial axis joining 0 to 180° is a 45° clockwise rotation of the line of identity in the four-quadrant plots, and represents agreement. The better the agreement between Δ EELV measurements, the closer data pairs will lie along the horizontal radial axis. The distance from the center of each plot represents the mean change in EELV between methods (mean Δ EELV) at each consecutive time point. Data points located between 315° and 45° refer to time points in which both EELV_{CT} and EELV_{WI-WO} increased (upper right quadrant of the four quadrant plot), while data points located between 135° and 225° refer to consecutive time points in which both EELV_{CT} and EELV_{WI-WO} decreased (lower left quadrant of the four quadrant plot). Data points located between 45 and 135° or 225 and 315° correspond to disagreement in the directional change of EELV between the washin-washout technique and computed tomography. Continuous line represents the angular bias, while dashed lines represent radial limits of agreement. EELV_{WI-WO}, end-expiratory lung volume assessed with the nitrogen washin-washout technique; EELV_{CT}, end-expiratory lung volume assessed by computed tomography; Δ EELV, change in EELV between consecutive measurements.

preferentially directed toward non-overinflated regions and that overinflated regions may not be detected in the EELV measurement. However, this explanation is not supported by our data, since the amount of overinflated area was very low even at the highest PEEP level in our study (1.1 ± 0.89 mL). Nevertheless, the observed difference in EELV between methods at high PEEP may be related to the fact that the WI-WO method measures a functional EELV, while CT measures anatomical EELV. Occurrence of leaks at high PEEP is another hypothesis to explain the non-constant bias, but this explanation is unlikely since plateau pressure was maintained during the prolonged end-inspiratory pauses performed for CT acquisition. Finally, there may be insufficient nitrogen mixing within the aerated lung, during the time allocated for measurement by the ventilator; since animals were ventilated at high RR and low V_T , which may have increased the time to reach equilibrium during the WI-WO measurement. An extended time between experimental stages and/or a lengthened WI-WO period may have narrowed the bias between methods.

Regarding precision, comparison between aforementioned studies, using limits of agreement is hindered by heterogeneity of EELV values across studies. Assessment of percentage error may overcome this problem, but was unavailable in the two previously published studies [2,19]. Using Data Thief 3.0 to extract Cartesian data from these studies, we have computed from the author's published figures, the percentage error which amounted to 28% in the human study and 46% in the pig study, versus 57% in our

Table 3 Diagnostic performance of EELV_{WI-WO} to detect variations in EELV_{CT} at different thresholds

Δ EELV _{CT} threshold for AUC computation (mL)	AUC (CI 95%)	Optimal Δ EELV _{WI-WO} cut-off (mL)	Se	Sp	PPV	NPV	PLR	NLR	Youden index
100	0.58 (0.50 to 0.66)	42	0.84	0.33	0.57	0.66	1.25	0.48	0.17
150	0.73 (0.64 to 0.81)	166	0.65	0.75	0.46	0.87	2.61	0.47	0.40
200	0.79 (0.70 to 0.89)	166	0.80	0.75	0.42	0.94	3.26	0.27	0.55
250	0.87 (0.79 to 0.94)	169	0.90	0.77	0.41	0.97	3.89	0.13	0.67
300	0.89 (0.83 to 0.95)	169	0.93	0.77	0.41	0.98	4.05	0.09	0.70

AUC, area under receiver operating characteristic curve; CI 95%, 95% confidence interval; Δ EELV_{CT}, absolute change in end-expiratory lung volume assessed by computed tomography between consecutive time points; Δ EELV_{WI-WO}, absolute change in end-expiratory lung volume assessed with the nitrogen washin-washout technique between consecutive time points; NLR, negative likelihood ratio; NPV, negative predictive value; PLR, positive likelihood ratio; PPV, positive predictive value; Se, sensitivity, Sp, specificity.

study. The relatively lower precision computed from our data may be a consequence of ventilatory settings, that may have particularly challenged the validity of the WI-WO technique. Indeed, FiO_2 greater than 0.7 precludes the computation of the respiratory quotient (RQ) required for EELV measurements, and a default RQ of 0.85 is assumed by the Engström Carestation® ventilator.

However, using a metabolically active lung model, Olegard et al. have nicely demonstrated that errors in RQ computation have a negligible effect on the precision of EELV measurements [1], suggesting that the high FiO_2 used in our study may have only marginally influenced our results. Regarding trending, the lack of significant angular bias suggests that calibration of $\text{EELV}_{\text{WI-WO}}$ is in agreement with the reference method. However, the relatively wide radial limits of agreement suggest that external factors may account for the variability of the relationship between $\Delta\text{EELV}_{\text{WI-WO}}$ and $\Delta\text{EELV}_{\text{CT}}$. We could speculate that this phenomenon is mainly related to the effect of PEEP on the bias between $\text{EELV}_{\text{WI-WO}}$ and $\Delta\text{EELV}_{\text{CT}}$.

Our study has several strengths. Since multiple combinations of PEEP and V_T were evaluated, a systematic analysis of the effect of ventilator parameters on the reliability of the technique could be performed using multivariate analysis, and was able to identify the PEEP level as an independent risk factor for measurement error. Furthermore, this is the first study having assessed trending ability of the WI-WO technique, and provided with cut-off values above which EELV changes may be considered as meaningful. Finally, the present study, while performed with particularly challenging ventilatory settings (high FiO_2 , high PEEP, high RR, and low V_T), demonstrates that the validity of the WI-WO technique may be extended to the sickest ARDS patients.

Our study has nevertheless some methodological issues that must be addressed. First, it was conducted using pediatric sensors for $\text{EELV}_{\text{WI-WO}}$ measurements, which may be less accurate for the highest V_T . Nevertheless, a subset analysis after exclusion of $V_T > 300$ mL led to similar results (Additional file 3: Figure S1). Furthermore, the bias was not increased at high V_T , as compared to low V_T , as shown by our interaction plot (Figure 4). Another limitation, in the perspective of extrapolation of these results to ARDS patients, is related to the relatively low EELV achieved in the pigs of this study in some experimental conditions. However, 62% of the EELV_{CT} measurements were greater than the first EELV quartile observed at low PEEP in a recent study on 30 ARDS patients [23], suggesting that most of the measurements performed in our study are in the range of clinically plausible values for EELV in ARDS patients. Another potential limitation is that the ARDS model used in the present study is particularly recruitable with PEEP. However, 50% of ARDS patients are considered recruiters by PEEP [23,25], and early ARDS share similar features as saline lavage regarding response to PEEP. The 2-min interval between V_T changes and EELV measurements may have been too short for CO_2 equilibration and achievement of both progressive recruitment and blood flow redistribution. However, a subset analysis limited to data acquired during the PEEP trial (with 10 min between measurements) led to similar results (see Additional file 4: Figure S2).

The present study may have important clinical implication. Indeed, as shown in Table 3, a change in $\text{EELV}_{\text{WI-WO}}$ greater than 166 mL would give an important clue to the clinician that the true EELV has changed by more than 200 mL. Furthermore, despite the non-constant bias of the EELV measurement by the WI-WO technique, the

true EELV value may still be assessed using Equation 1, provided that the absolute EELV value is relevant for the clinician [24].

Conclusion

The reliability of the WI-WO technique is critically dependent on ventilatory settings, but sufficient to accurately detect EELV change over time greater than 200 mL.

Additional files

Additional file 1: Table S1. Reasons for lack of data as a function of each of the 3 experimental stages. Values are number of lacking data/total number of data (%). $EELV_{WI-WO}$, end-expiratory lung volume assessed with the nitrogen washout-washin technique; $EELV_{CT}$, end-expiratory lung volume assessed by computed tomography; V_T , tidal volume.

Additional file 2: Table S2. Ventilatory settings and arterial blood gases in each experimental condition. Values are number of mean \pm standard deviation (range). ALI, acute lung injury onset; PEEP, positive end-expiratory pressure; RR, respiratory rate; V_T , tidal volume.

Additional file 3: Figure S1. Bias and limits of agreement between $EELV_{CT}$ and $EELV_{WI-WO}$, using Bland and Altman representation in a subset of the data (exclusion of $V_T > 300$ mL). Each symbol represents a concomitant measurement of $EELV_{WI-WO}$ and $EELV_{CT}$. Horizontal continuous line and horizontal broken lines are the mean bias and 95% prediction interval limits of the bias between $EELV_{WI-WO}$ and $EELV_{CT}$, respectively. $EELV_{WI-WO}$, end-expiratory lung volume assessed with the nitrogen washout-washin technique; $EELV_{CT}$, end-expiratory lung volume assessed by computed tomography; 95% p.i., 95% prediction interval of the bias between $EELV_{WI-WO}$ and $EELV_{CT}$; V_T , tidal volume.

Additional file 4: Figure S2. Bias and limits of agreement between $EELV_{CT}$ and $EELV_{WI-WO}$, using Bland and Altman representation in a subset of the data, acquired during the PEEP trial (with 10 min between measurements). Each symbol represents a concomitant measurement of $EELV_{WI-WO}$ and $EELV_{CT}$. Horizontal continuous line and horizontal broken lines are the mean bias and 95% prediction interval limits of the bias between $EELV_{WI-WO}$ and $EELV_{CT}$, respectively. $EELV_{WI-WO}$, end-expiratory lung volume assessed with the nitrogen washin-washout technique; $EELV_{CT}$, end-expiratory lung volume assessed by computed tomography; 95% p.i., 95% prediction interval of the bias between $EELV_{WI-WO}$ and $EELV_{CT}$; V_T , tidal volume.

Abbreviations

ARDS: acute respiratory distress syndrome; AUC: area under curve; $\Delta EELV_{WI-WO}$: change in end-expiratory lung volume between consecutive measurements by the nitrogen washin-washout technique; $\Delta EELV_{CT}$: change in end-expiratory lung volume between consecutive measurements by computed tomography; EELV: end-expiratory lung volume; $EELV_{WI-WO}$: end-expiratory lung volume measurement by the nitrogen washin-washout technique; $EELV_{CT}$: end-expiratory lung volume measurement by computed tomography; FiO_2 : fraction of inspired oxygen; PEEP: positive end-expiratory pressure; RR: respiratory rate; SD: standard deviation; V_T : tidal volume; WI-WO: nitrogen washin-washout.

Competing interests

JCR, CP, AMP, JST, MO, BN, MHH, and FL have no competing interests. CG received a grant of 9600 € by GE Healthcare as study funding. CG has no other ties with this company, and the manuscript was submitted without review by this company.

Authors' contributions

JCR and CG have made substantial contributions to the conception, design, acquisition of data, and analysis and interpretation of data; AMP, JST, MO, BN, and MHH to the analysis and interpretation of data; MO to the conception, design, and analysis and interpretation of data; CP to the conception, acquisition of data, and analysis and interpretation of data; and FL to the acquisition of data. JCR has drafted the submitted article. CP, AMP, JST, MO, BN, MHH, FL, and CG have revised the draft critically for important intellectual content. All authors have provided the final approval of the version to be published; and agreed to be accountable for all aspects of the work in ensuring that questions related to the accuracy or integrity of any part of the work are appropriately investigated and resolved.

Role of the sponsors

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References

1. Olegard C, Sondergaard S, Houltz E, Lundin S, Stenqvist O (2005) Estimation of functional residual capacity at the bedside using standard monitoring equipment: a modified nitrogen washout/washin technique requiring a small change of the inspired oxygen fraction. *Anesth Analg* 101:206–212
2. Chiumello D, Cressoni M, Chierichetti M, Tallarini F, Botticelli M, Berto V, Mietto C, Gattinoni L (2008) Nitrogen washout/washin, helium dilution and computed tomography in the assessment of end expiratory lung volume. *Crit Care* 12:R150
3. Dellinger RP, Levy MM, Rhodes A, Annane D, Gerlach H, Opal SM, Sevransky JE, Sprung CL, Douglas IS, Jaeschke R, Osborn TM, Nunnally ME, Townsend SR, Reinhart K, Kleinpell RM, Angus DC, Deutschman CS, Machado FR, Rubenfeld GD, Webb S, Beale RJ, Vincent JL, Moreno R, Surviving Sepsis Campaign Guidelines Committee including The Pediatric Subgroup (2013) Surviving sepsis campaign: international guidelines for management of severe sepsis and septic shock, 2012. *Intensive Care Med* 39:165–228
4. Sondergaard S, Karason S, Wiklund J, Lundin S, Stenqvist O (2003) Alveolar pressure monitoring: an evaluation in a lung model and in patients with acute lung injury. *Intensive Care Med* 29:955–962
5. Top A, Hamarneh G, Abugharbieh R (2011) Spotlight: Automated Confidence-Based user Guidance for Increasing Efficiency in Interactive 3D Image Segmentation. In: Menze B, Langs G, Tu Z, Criminisi A (ed) *Medical Computer Vision, Recognition Techniques and Applications in Medical Imaging*. Springer Berlin Heidelberg, Berlin Heidelberg, p 204
6. Top A, Hamarneh G, Abugharbieh R (2011) Active Learning for Interactive 3D Image Segmentation. In: Fichtinger G, Martel A, Peters T (ed) *Medical Image Computing and Computer-Assisted Intervention – MICCAI 2011*. Springer Berlin, Heidelberg
7. Attinger EO, Cahill JM (1960) Cardiopulmonary mechanics in anesthetized pigs and dogs. *Am J Physiol* 198:346–348
8. Acute Respiratory Distress Syndrome Network (2000) Ventilation with lower tidal volumes as compared with traditional tidal volumes for acute lung injury and the acute respiratory distress syndrome. *N Engl J Med* 342:1301–1308
9. R Core Team (2013) R: a Language and Environment for Statistical Computing. R Foundation for statistical Computing, Vienna, Austria. <http://cran.r-project.org>
10. Pinheiro J, Bates D, Debroy S, Sarkar D, The R Development Core Team (2013) nlme: Linear and Nonlinear Mixed Effects Models. <http://cran.r-project.org/web/packages/nlme/index.html>
11. Carstensen B, Gurrin L, Ekstrom C, Figurski M (2013) MethComp: Functions for Analysis of Agreement in Method Comparison Studies. <http://cran.r-project.org/web/packages/MethComp/index.html>
12. Robin X, Turck N, Hainard A, Tiberti N, Lisacek F, Sanchez J-C, Müller M (2011) pROC: an open-source package for R and S + to analyze and compare ROC curves. *BMC Bioinforma* 12:77
13. Lopez-Raton M, Rodriguez-Alvarez MX (2012) Optimal Cutpoints: Computing Optimal Cutpoints in Diagnostic Tests. <http://cran.r-project.org/web/packages/OptimalCutpoints/index.html>
14. Hothorn T, Bretz F, Westfall P (2008) Simultaneous inference in general parametric models. *Biom J* 50:346–363
15. Bland JM, Altman DG (2007) Agreement between methods of measurement with multiple observations per individual. *J Biopharm Stat* 17:571–582
16. Carstensen B (2011) *Comparing Clinical Measurement Methods: a Practical Guide (Statistics in Practice)*, 2nd edition. Wiley, Chichester
17. Carstensen B, Simpson J, Gurrin LC (2008) Statistical models for assessing agreement in method comparison studies with replicate measurements. *Int J Biostat* 4:1–26
18. Critchley LA, Critchley JA (1999) A meta-analysis of studies using bias and precision statistics to compare cardiac output measurement techniques. *J Clin Monit Comput* 15:85–91
19. Graf J, Santos A, Dries D, Adams AB, Marini JJ (2010) Agreement between functional residual capacity estimated via automated gas dilution versus via computed tomography in a pleural effusion model. *Respir Care* 55:1464–1468
20. Tummers B (2006) Datathief III. <http://datathief.org>
21. Critchley LA, Lee A, Ho AM-H (2010) A critical review of the ability of continuous cardiac output monitors to measure trends in cardiac output. *Anesth Analg* 111:1180–1192
22. Critchley LA, Yang XX, Lee A (2011) Assessment of trending ability of cardiac output monitors by polar plot methodology. *J Cardiothorac Vasc Anesth* 25:536–546
23. Dellamonica J, Lerolle N, Sargentini C, Beduneau G, Di Marco F, Mercat A, Richard JC, Diehl JL, Mancebo J, Roubey JJ, Lu Q, Bernardin G, Brochard L (2011) PEEP-induced changes in lung volume in acute respiratory distress syndrome. Two methods to estimate alveolar recruitment. *Intensive Care Med* 37:1595–1604
24. Bland JM, Altman DG (1999) Measuring agreement in method comparison studies. *Stat Methods Med Res* 8:135–160
25. Gattinoni L, Caironi P, Cressoni M, Chiumello D, Ranieri VM, Quintel M, Russo S, Patroniti N, Cornejo R, Bugego G (2006) Lung recruitment in patients with the acute respiratory distress syndrome. *N Engl J Med* 354:1775–1786

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