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**LIPID NANOCAPSULES LOADED WITH AN ORGANOMETALLIC TAMOXIFEN
DERIVATIVE AS A NOVEL DRUG-CARRIER SYSTEM FOR EXPERIMENTAL
MALIGNANT GLIOMAS**

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ABSTRACT

Ferrocenyl diphenol tamoxifen derivative (Fc-diOH) is one of the most active molecules of a new class of organometallic drugs, showing *in vitro* antiproliferative effects on both hormone-dependent and independent breast cancer cells. For the first time, Fc-diOH was tested on a 9L glioma model according to two encapsulation strategies: lipid nanocapsules (LNC) and swollen micelles. LNC showed a higher drug loading capacity because of a larger oily core in their structure and were able to be up taken by glioma cells. The large amount of PEG present at the micellar interface prevented interaction with cytoplasm membrane which led to a low level of micelle cell uptake and no biological activity. On the contrary, Fc-diOH cytostatic activity was conserved after its encapsulation in LNC and was very effective on 9L-glioma cells as the IC_{50} was about $0.6\mu M$. Interestingly, Fc-diOH-loaded LNC showed low toxicity levels when in contact with healthy cells, conferring a functional specificity of this compound on tumour cells. Finally, Fc-diOH LNC treatment was able to lower significantly both tumour mass and volume evolution after 9L-cell implantation into rats which evidenced for the first time the *in vivo* efficacy of this new kind of organometallic compound.

Keywords: Lipid nanocarrier, organometallic compound, cell uptake, drug delivery, 9L tumour model

1. INTRODUCTION

Gliomas are the most common type of primary brain tumours. The prognosis for patients with glioblastoma, the most aggressive type of brain malignancy, has remained largely unchanged over the last three decades. Recent studies give a median survival time of 14.6 months for patients treated with radiotherapy plus temozolomide, which is the reference chemotherapy, and 12.1 months with radiotherapy alone [1]. Clearly, new and effective therapies are desperately awaited.

Tamoxifen, a member of the Selective Estrogen Receptor Modulator (SERM) family, has been widely used in the treatment of estrogen receptor (ER)-expressing breast cancer [2-4]. Because antitumour effects have been predominantly observed in patients with ER-positive tumours, it is generally accepted that the primary action of hydroxytamoxifen, its active metabolite, is mediated through inhibition of the ER pathway. But, it has previously been shown that some ER-negative cancers also respond to tamoxifen, [5, 6] which means that the molecule can be active because of an ER-independent antitumour mechanism that has not yet been clearly identified [7]. Taking into account that gliomas are ER-negative [8-10], the moderate beneficial effect of tamoxifen in glial neoplasms has been linked to an ER-independent antitumour mechanism. For the treatment of patients with recurrent malignant gliomas, only trials using high-dose tamoxifen alone or in combination with other cytotoxic agents have demonstrated positive results [11-13]. As a consequence, SERM represent a promising therapy for gliomas if their antitumour activity can be improved.

Previously, a potentially cytotoxic moiety, ferrocene, was incorporated into the tamoxifen skeleton [14]. A series of these molecules, called organometallic tamoxifen derivatives by analogy, were prepared and their cytotoxic effects were studied, initially on breast cell lines [15, 16]. By modifying various structural aspects of the ferrocenyl derivatives, one of the most

effective compounds to date in term of cytotoxicity is the ferrocenyl diphenol compound Fc-diOH (Fig. 1). This compound showed high levels of *in vitro* antiproliferative activity against both hormone-dependent (MCF7, $IC_{50} = 0.7\mu M$) and independent (MDA-MB231, $IC_{50} = 0.6\mu M$) breast cancer cell lines [16], and has become the standard to which the activity of novel organometallic anti-cancer drugs can be compared. The observed antiproliferative effect of these molecules can be divided into two actions: anti-oestrogenic in ER(+) cells and cytotoxic in both ER(+) and ER(-) cells. The efficacy of these drugs has been related to an activation pathway which involves the *in vitro* oxidation of the ferrocene and phenol functions [17, 18]. These organometallic tamoxifen derivatives could have an enormous impact on medicine, in particular in the treatment of cancer [19]. As demonstrated by Rosenberg's discovery of cisplatin [20] which revolutionized the treatment of testicular cancer, organometallic complexes can be a powerful weapon as antitumour agents [21].

In the present study, the antitumoural efficacy of Fc-diOH was tested on glioma cells. As this product is very hydrophobic, and since its water-insolubility can impede its potential biological activity [22], we aimed at developing a new way to administer this molecule. Two strategies were investigated: a ferrocenyl diphenol compound was encapsulated in lipid nanocapsules (LNC) for one strategy and in swollen micelles for another, according to an organic solvent-free process recently developed in our laboratory [23]. These lipid nanocarriers obtained by a low-energy emulsification method were characterised by the absence of organic solvent in their formulation. They presented a low particle size, ranging from 10 to 20nm for swollen micelles and from 20 to 100nm for LNC, with a narrow polydispersity size and the capacity to carry lipophilic molecules. Taking into account these various advantages, Fc-diOH-loaded nanocarriers were developed and tested on glioma culture cells and on a subcutaneous 9L-rat glioma model.

2. MATERIALS AND METHODS

2.1. Materials

Ferrocenyl diphenol compound (2-ferrocenyl-1,1-bis(4-hydroxyphenyl)-but-1-ene) named Fc-diOH was prepared by McMurry coupling [24]. Its purity was assessed by HPLC, NMR and elemental analysis. Hydroxytamoxifen, Ferrocene and Nile Red were supplied by Sigma-Aldrich (Saint Quentin Fallavier, France). The lipophilic Labrafac[®] CC (caprylic-capric acid triglycerides) was kindly provided by Gattefosse S.A. (Saint-Priest, France). Lipoid[®] S75-3 (soybean lecithin at 69% of phosphatidylcholine) and Solutol[®] HS15 (a mixture of free polyethylene glycol 660 and polyethylene glycol 660 hydroxystearate) were a gift from Lipoid GmbH (Ludwigshafen, Germany) and BASF (Ludwigshafen, Germany), respectively. NaCl, acetone, ethanol and tetrahydrofuran (THF) were obtained from Prolabo (Fontenay-sous-bois, France). Deionized water was obtained from a Milli-Q plus system (Millipore, Paris, France).

2.2. Preparation of Fc-diOH-loaded nanocarriers

Lipid nanocarriers were prepared according to a previously described original process [23]. In order to obtain LNC, Solutol[®] HS15 (17% w/w), Lipoid[®] (1.5% w/w), Labrafac[®] (20% w/w), NaCl (1.75% w/w) and water (59.75% w/w) were mixed and heated under magnetic stirring up to 85°C. Three cycles of progressive heating and cooling between 85 and 60°C were then carried out and followed by an irreversible shock induced by dilution with 2°C deionised water (45 or 70% v/v) added to the mixture at 70-75°C. To formulate Fc-diOH-loaded LNC, two parameters will be changed: the amount of Fc-diOH in triglycerides (1.7% and 4% (w/w))

and the volume of cold water for LNC dilution (70% and 45% v/v) for drug loading of 1mg/g (0.84% w/w dry weight) and 6.5mg/g (2% w/w dry weight) respectively.

To form swollen micelles, Solutol[®] HS15 (64.25% w/w), Labrafac[®] (5% w/w), NaCl (1.75% w/w) and water (29% w/w) were mixed and the same formulation flow chart was applied as previously described. To formulate Fc-diOH-loaded micelles 1mg/g (0.24% w/w dry weight), the amount of Fc-diOH in triglycerides was equivalent to 3.4% (w/w) and the volume of dilution was about 42% (v/v).

Fluorescent lipid nanocarriers were obtained by using Nile Red, an hydrophobic fluorescent marker, previously dissolved in acetone at 2µg/µl. The resulting Nile Red solution was incorporated in the triglyceride phase at 50:50 (w/w) and the acetone was evaporated before use. Fluorescent LNC and micelles were then prepared as described above.

2.3. Characterisation of the nanocarriers

2.3.1. Particle size and zeta potential

The nanocarriers were analysed for their size and charge distribution using a Malvern Zetasizer[®] Nano Serie DTS 1060 (Malvern Instruments S.A., Worcestershire, UK). The nanocarriers were diluted 1:100 (v/v) in deionised water in order to assure a convenient scattered intensity on the detector.

2.3.2. LNC drug payload and encapsulation efficiency

Because of the orange colour of the anticancer drug, the Fc-diOH payload was determined by spectrophotometry at 450nm after dissolving LNC and swollen micelles in solvent mixtures as described below. As the water solubility of Fc-diOH was inferior to 0.001µg/ml, if the product

was not entrapped in nanocarriers, drug precipitation occurred and the precipitate could be retained by a filter. Consequently, a part of the formulation of each batch was filtrated using a Minisart[®] 0.1- μ m filter (Sartorius). Three samples of each batch of Fc-diOH-loaded nanocarriers (filtrated and non-filtrated) were prepared by dissolving 250mg of nanocarriers in 2.25ml of 22/67/11 (v/v/v) acetone/THF/water solution. Quantification was achieved by comparing the absorbency of ferrocenyl derivative samples to a calibration curve made with blank nanocarriers and Fc-diOH ethanol/THF/water solution. Mean drug payload (milligrams of drug per gram of LNC dispersion or micellar solution) and encapsulation efficiency (%) were calculated.

2.4. Cell experiments

2.4.1. Cell culture

Rat 9L gliosarcoma cells were obtained from the European Collection of Cell Culture (Salisbury, UK, N^o94110705). Purified newborn rat primary astrocytes were obtained by the mechanical dissociation method from cultures of cerebral cortex as originally described [25]. The cells were grown at 37°C/5% CO₂ in Dulbecco modified Eagle medium (DMEM) with glucose and L-glutamine (BioWhittaker, Verviers, Belgium) containing 10% foetal calf serum (FCS) (BioWhittaker) and 1% antibiotic and antimycotic solution (Sigma, Saint-Quentin Fallavier, France).

2.4.2. Observation of nanocarrier internalisation by confocal images

9L cells were plated at 10⁴/ml on 24-well plates covered with 14mm microscope cover glasses coated with a solution of 5 μ g/ml in PBS of poly-D-lysine hydrobromide mol wt 70,000-150,000 (Sigma, Saint-Quentin Fallavier, France). After 48h of culture, the culture medium

was removed and changed to a serum-free medium containing 50% DMEM, 50% Ham's F12 and N1 complement. At Day 3, the medium was totally removed and the cells were incubated for 2 hours with a medium containing the medium alone as a negative control, fluorescent LNC 1:1,000 or fluorescent micelles 1:1,000. The cells were then washed twice with Hanks balanced salt solution (HBSS, BioWhittaker) and fixed with 4% paraformaldehyde in PBS for 15 minutes at 4°C. They were washed three times with HBSS, the cover glasses were removed and finally mounted on slides in glycerol/PBS 1:1. The cells and fluorescent nanocarriers were observed by confocal microscopy (Olympus light microscope Fluoview FU 300 Laser Scanning Confocal Imaging System, Paris, France) with a helium-argon laser (λ_{ex} : 543nm, λ_{em} : 572nm). The morphology of the 9L cells was shown by Nomarsky contrast.

2.4.3. Quantification of nanocarrier internalisation by flow cytometry

A BD FACSCalibur fluorescent-activated flow cytometer and the BD CellQuest software (BD Biosciences, Le Pont de Claix, France) were used to perform flow cytometry analysis. Nile Red-loaded micelles (1/1,000) and Nile Red-loaded LNC (1/1,000) were incubated with 9L glioma cells in a serum-free medium containing 50% DMEM, 50% Ham's F12 (Biowhittaker) and N1 complement (Sigma). After 2 hours of incubation, the removal of the attached nanocarriers was accomplished by washing the cells three times with HBSS. The cells were then detached by trypsinisation. After centrifugation, they were resuspended in a 0.4% (w/v) Trypan Blue solution in HBSS to quench the extracellular fluorescence, thus enabling the determination of the fraction that was actually internalised. The treated samples were subsequently washed twice, and analysed by flow cytometry in at least triplicate experiments, with 10,000 cells being measured in each sample. For quantification analysis, no treatment (9L cells) was considered to be the 100% of fluorescence intensity.

2.4.4. *In vitro* cell viability

The cells were first plated at 10^4 cells/mL on 24-well plates for 48h in DMEM containing 10% FCS and 1% antibiotic/antimycotic and then treated with increasing concentrations of various preparations. To test the impact of the drug alone (non encapsulated) on cells, solvent like ethanol (for Fc-diOH and OH-Tam) and acetone (for Fc) were used to solubilise the drugs. Drug in solution were prepared at a concentration of 0.1 M and a dilution of 1:1,000 in culture medium was realised to obtain the higher concentration tested on cells (100 μ mol/L). To test drugs encapsulated in micelles or in LNC at this concentration, a dilution of 1: 23.5 was realised in culture medium. For the others concentrations, 1: 10 cascade dilution was performed. Blank LNC and micelles were tested as controls and with the same excipient concentration than that needed for Fc-diOH ones. The cells were incubated at 37°C/5% CO₂ for 96h. Thereafter, cell viability was determined by the MTT test according to the procedure described by Mosmann [26]. Briefly, 40 μ l of MTT solution at 5mg/ml in PBS 1X were added to each well, and the plates were incubated at 37 °C for 4h. The medium was removed and 200 μ l of acid–isopropanol 0.06N was added to each well and mixed thoroughly to completely dissolve the dark blue crystals. The optical density values were measured at 580nm using a multiwell-scanning spectrophotometer (Multiskan Ascent, Labsystems SA, Cergy-pontoise, France). Two independent repetition experiments are conducted, each with a least 6 repeated samples.

2.5. Animal study

2.5.1. Animals and anaesthesia

Syngeneic Fischer F344 female rats weighing 160-175g were obtained from Charles River Laboratories France (L'Arbresle, France). All experiments were performed on 10 to 11-week

old female Fisher rats. The animals were manipulated under isoflurane/oxygen anesthesia. Animal care was provided in strict accordance to French Ministry of Agriculture regulations.

2.5.2. Tumour and nanocarrier implantation

A cultured tumour monolayer was detached with trypsin-ethylene diamine tetraacetic acid, washed twice with EMEM without FCS or antibiotics, counted, and resuspended to the final concentration desired. For tumour growth analysis, animals received subcutaneous injections (s.c) of 1.5×10^6 9L cells into the right thigh. On Day 6 after cell injection, rats implanted with 9L cells were treated by an intratumoural (i.t) single injection (400 μ l) of different treatments. Group 1 was injected with physiological saline (control; n = 7 animals), Group 2 received blank LNC (n = 7 animals), Group 3 received Fc-diOH-loaded micelles 1mg/g (2.5 mg/kg; n = 8 animals), Group 4 received Fc-diOH-loaded LNC 1mg/g (2.5mg/kg; n = 8 animals) and Group 5 was treated with Fc-diOH-loaded LNC at a higher dose of 6.5mg/g (16.2 mg/kg; n = 5 animals). The length and width of each tumour were regularly measured using a digital caliper, and tumour volume was estimated with the mathematical ellipsoid formula given in equation (1). At the end of the study (Day 30), the rats were sacrificed and the weight of each tumour was evaluated.

$$\text{Volume (V)} = (\pi/6) \times \text{width}^2 (l) \times \text{length (L)} \quad (1)$$

2.6. Statistical analysis

For *in vitro* cell survival tests, statistics and analysis of the Similarity Factor f_2 were employed to evidence significant curve profiles ($f_2 < 50$ was considered to be significant). The statistical significance for the *in vivo* study was determined for each experiment between groups by a student t-test ($P < 0.05$ was considered to be significant).

3. RESULTS AND DISCUSSION

3.1. Preparation and characterisation of Fc-diOH-loaded nanocarriers

By mixing Fc-diOH with excipients at well-characterised concentrations described by a ternary diagram [23] and by applying the phase inversion process, lipid nanocapsules and swollen micelles loaded with Fc-diOH were obtained. LNC loaded with the anticancer drug presented a very narrow size between 44.7 and 51.7nm, depending on the drug payload, and were monodispersed ($PI < 0.15$) (Table 1). Fc-diOH-loaded LNC were also characterised in term of surface charge. Zeta potential values ranged from -10.0 to -11.5mV. The physicochemical properties were very similar to previously-studied standard blank LNC [27, 28]. Indeed, because of the presence of PEG dipoles in their shells, 50nm blank LNC have a low zeta potential of approximately -10mV [29]. The presence of the active drug did not affect the zeta potential value which means that the entrapment of Fc-diOH was very efficient. Due to the nearly negligible solubility of ferrocenyl compound in water and its high solubility in triglycerides (Labrafac[®]), it was possible to reach high drug loading levels, up to 6.5mg of Fc-diOH per gram of LNC suspension (2% w/w dry weight). Like many hydrophobic drugs [30-32], Fc-diOH was well-encapsulated in LNC with a high encapsulation efficiency above 98% (Table 2).

Due to a low quantity of triglycerides present in swollen micelles and because of the limit of solubility for Fc-diOH in triglycerides, it was only possible to obtain micelles with a drug load equivalent to 1mg/g (0.24% w/w dry weight). Nevertheless, they were obtained with the same size and zeta potential as blank micelles (Table 1). The Fc-diOH-loaded micelles were characterised by a very small particle size, $13.2 \pm 0.3\text{nm}$, the same as for blank ones ($13.0 \pm 0.1\text{nm}$) and exhibited a very weak negative charge with values around -2mV. The

incorporation of Fc-diOH in swollen micelles was very effective, as demonstrated by the high encapsulation efficiency and the stability of the zeta potential (Tables 1&2).

3.2. Cell line experiments

3.2.1. Nanocarrier cell uptake

The internalisation of lipid nanocarriers in glioma cells was investigated by confocal microscopy and flow cytometry after the formulation of Nile Red (NR)-loaded LNC and micelles. As their size and charge measurements were very similar to those of blank nanocarriers (Table 1), NR-loaded LNC and micelles were considered to mimic the behaviour of nanocarriers entrapping the anticancer drug. Quantitative cellular uptake by FACS analysis (Fig. 2) and images taken after the incubation of fluorescent nanocarriers with 9L cells (Fig. 3) showed that there was a significant difference between the two nanocarriers in terms of cell uptake. Fig. 2A shows that LNC were rapidly taken up by 9L cells. Cell fluorescence intensity increased from 100% for cells alone (control) to 354.4% for cells incubated with NR-LNC (Fig. 2B). As seen in Fig. 3A, all the fluorescence was found inside the cell, while avoiding the nucleus, demonstrating an uptake of the nanocapsules. This uptake could be attributed to the interactions between 50nm LNC and cholesterol-rich microdomains as previously observed [33]. On the contrary, a very weak level of fluorescence was observed after the incubation of Nile Red-loaded micelles with 9L cells which means that only a few micelles are able to penetrate the cells (Fig. 3B). Cytometry results confirmed that fluorescent micelles were taken up by 9L cells at much lower levels than LNC (205.2%) (Fig. 2B). Dunn *et al.* investigated the effect of an increased surface density of PEG with constant chain length, on the uptake of pegylated nanoparticles by non-parenchymal liver cells. The interaction of the particles with cells was shown to decrease as the surface density of PEG increased [34]. The

surfactant barrier in swollen micelles was more than 7 times higher in proportion to those used for LNC formulations for the same drug load. So, whereas micelles are smaller than LNC, the presence of high density PEG coating certainly decreased interaction with cells and could be responsible of the low internalisation of swollen micelles in 9L glioma cells. Moreover, when the concentration of Solutol[®] HS15 was above its CMC (0.03% w/v), the amount of colchicine taken up into rat hepatocytes, as well as its uptake velocity, were significantly decreased [35]. This phenomenon was explained by an inhibition of colchicine transport either due to direct interaction at the transport site or due to alteration of membrane properties in the presence of Solutol[®] HS15 micelles.

3.2.2. Cell viability

Fc-diOH was tested *in vitro* in a survival assay on 9L glioma cell and on newborn rat astrocyte primary cultures. Ferrocene (Fc) and hydroxytamoxifen (OH-Tam), which are the main molecules of the Fc-diOH structure, were also tested. No toxic effect was observed for the ethanol/acetone solutions used to solubilise drugs in solution (data not shown). Glioma cell culture studies revealed that a distinct and large decrease in cancer cell viability could be achieved with Fc-diOH, contrary to OH-Tam and Fc (Fig. 4A). The IC₅₀ for Fc-diOH was about 0.5 μM whereas OH-Tam was totally inactive at this concentration range (IC₅₀ = 35 μM). Similar results had already been found in MDA-MB231 cells which are classified as ER(-) breast cancer cell lines, since the IC₅₀ for ferrocenyl tamoxifen derivative and OH-Tam were about 0.5 μM [36] and 34 μM respectively [37, 38]. Tamoxifen, the reference molecule of the SERM family, is well known to act through its inhibition of ER. However, it has been already described that the oxidation of tamoxifen to quinoids is a recognised pathway of cytotoxicity [39, 40]. As glioma cells are classified as ER(-) cell lines [9], the moderate effect of tamoxifen

on 9L cells can be attributed to its oxidant activity. Furthermore, ferrocene was totally inactive on 9L cells. The same result has already been observed on ER(+) and ER(-) breast cell lines [15], even though it showed some antitumour potential, though at high concentrations (10^{-4} M), when oxidized into the ferrocenium ion [41]. The fact that Fc-diOH showed cytotoxic activity at much lower concentrations than OH-Tam suggests that the Fc group has a role in the observed cytotoxic effect. The easier oxidation of ferrocene in comparison to phenol, makes the oxidative metabolism of ferrocenyl derivatives easier, and consequently leads to better antiproliferative activity. As shown in Figure 4B, in astrocyte cells which are slow- or non-dividing cells, Fc-diOH at equivalent doses to those added to glioma cells demonstrated a largely reduced level of cell toxicity ($IC_{50} = 50\mu\text{M}$) equivalent to OH-Tam, whereas ferrocene was characterised overall by a total absence of cytotoxicity. These results indicate that Fc-diOH is toxic to brain tumour cells with a high potential for cell division, and harmless towards healthy cells.

Cell survival curves were not significantly different between Fc-diOH in solution and Fc-diOH-loaded LNC, showing that the activity of the drug was totally recovered *in vitro* after encapsulation (Fig. 4C). Moreover, Fc-diOH-loaded LNC demonstrated cytotoxic activity on 9L cells 150-fold higher than blank LNC. Taking into account the cytotoxic mechanism of ferrocenyl molecules proposed by Hillard *et al.* [17], these results suggest that LNC improved intracellular bioavailability of Fc-diOH. Indeed, it was demonstrated that upon electrochemical oxidation of the ferrocene group, a partial positive charge is imparted to the hydroxyl group of the molecule, thus acidifying the proton, which may then be easily abstracted by basic species like DNA, glutathione (GSH), or proteins, only present in the intracellular compartment. In a subsequent second oxidative step, quinone methide is formed,

and is activated for nucleophilic attack by sulphur and nitrogen donor groups from biomolecules which may lead to cell death. Furthermore, an advantageous effect was found for Fc-diOH when in contact with astrocytes (Fig. 4D). In fact, Fc-diOH in solution or entrapped in LNC, was found to be much less cytotoxic on astrocytes compared to cancer cells. The higher cytotoxic effect of Fc-diOH-loaded LNC in glioma cells than in astrocytes could be triggered by easier accessibility of the intracellular target during cell division. Additionally, astrocytes are considered to play an important role in the defence of the brain against reactive oxygen species (ROS) [42]. They are known to contain higher levels of various antioxidants, especially GSH, than other brain cell types like neurons and oligodendrocytes [43-45]. As GSH may be a potential target of the ferrocenyl tamoxifen derivatives, it can explain the reduced cell death of Fc-diOH on astrocytes. The higher cytotoxic effect of Fc-diOH-loaded LNC on glioma cells than on astrocytes cannot be explained by increased endocytosis during cell division, since LNC uptake is quantitatively equivalent in the two types of cells (A. Paillard *et al.*, unpublished observation). Consequently, Fc-diOH can be considered as a cytostatic anticancer molecule from an *in vitro* concentration of 0.5-0.6 μ M.

The results obtained with Fc-diOH-loaded micelles were different (Fig. 4E-F). Firstly, the activity of Fc-diOH in solution was not recovered after its encapsulation in swollen micelles. Moreover, there was no significant difference between blank and Fc-diOH-loaded micelles on 9L cell survival percentage, which means that the observed toxicity was related to the nanocarrier and not to the anticancer drug. The toxicity of swollen micelles was certainly due to the presence of excipients, especially surfactant molecules like Solutol[®]. In fact, the use of Solutol[®] HS15 in pharmaceutical preparations for *in vitro* applications should be considered

with care. Woodcock *et al.* studied the toxicity of different surfactants on cells and their capability to reverse multidrug resistance (MDR) [46]. Concerning Solutol[®] HS15, they concluded that 2/3 of the R100 cells (MDR-derivative of human leukaemia cell line) were lysed when incubated for only 1 hour with this polyethoxylated solubilising agent at concentrations equivalent to 1:100 (w/v) and 100% were lysed by 1:10 (w/v). Despite lower concentration of Solutol[®] HS15 in our micelles (0.037%), toxicity on 9L glioma cells was noted for blank micelles after 2 hours of incubation. In addition, swollen micelles were found to be toxic on healthy cells as well as on cancer cells as the IC₅₀ was about 5µM on both cell types (Fig. 4F). The cytotoxic activity of Fc-diOH on 9L decreased dramatically when it was encapsulated in micelle which confirms that swollen micelles were poorly internalised in 9L cells.

3.3. *In vivo* study

A 9L subcutaneous glioma model was used to evaluate the efficacy of Fc-diOH LNC and micelles. After tumours had developed to about 100mm³, we performed comparative efficacy studies by dividing animals into five groups according to the treatment they received. Rats were separated in random samples in a way to minimize weight and tumour size differences among the groups. Rats of the control and LNC groups were characterised by a very quick progression of tumour volume which reached 2,500 and 2,000mm³ by Day 30, respectively. (Fig. 5). On the contrary, Fc-diOH-loaded LNC significantly inhibited tumour growth ($p < 0.05$) which means that the cytostatic activity of Fc-diOH was preserved *in vivo*. Indeed, rats treated with a single injection of LNC at an equivalent dose of 2.5mg/kg presented tumours three times smaller (700mm³ at Day 30) than the ones treated by blank LNC (Fig. 5A). In contrast, rats treated by Fc-diOH-loaded micelles with the same anticancer drug dose had

tumours that grew very quickly and reached 1,600mm³ by the end of the study. These *in vivo* data can be linked to the conclusions made about nanocarrier uptake in 9L cells as an intratumoural treatment with Fc-diOH-loaded micelles was less effective than Fc-diOH-loaded LNC injection. Similarly, tumour growth assessed by tumour mass at the end of the study showed that the mean tumour mass had significantly decreased from 1.1 to 0.6g for 1mg/g loaded swollen micelles and LNC, respectively (Fig. 5B).

Nevertheless, no dose effect was evidenced as rats treated with Fc-diOH-loaded LNC at an equivalent dose of 16.2 mg/kg (6.5mg/g load) had s.c. tumour growth similar to LNC ones at an equivalent dose of 2.5mg/kg (1 mg/g load). The systematic diminution of size observed for 6.5mg/g-loaded LNC (44.7nm as opposed to 51.3 or 51.7nm for 1mg/g and 0.5mg/g, respectively, see Table 1) could be due to an intramolecular association between Fc-diOH molecules at this concentration which could explain the absence of dose effect. Moreover, a loss of Fc-diOH oxidative activity during the solubilising step using ultrasound or during the LNC formulation is not impossible. The phenol functions of two nearby molecules could react together leading to the unavailability of the pattern ferrocene-C=C-phenol required for internal electron-transfer. The protection of these phenol functions by grafting an acetate chain in order to make a prodrug, so that hydrolysis takes place *in situ*, should allow prolonged activity of Fc-diOH-loaded LNC. Work on this protection is in progress. Finally, it is also possible that the maximum effective dose was already reached with 1 mg/g loaded LNC (0.84% w/w dry weight) but that, as intratumoural administration does not permit to target all the disseminated cells, a unique injection may not be sufficient to provide the right dose at the right time. Extensive research is still required to optimise administration conditions for effective tumour reduction in rats.

4. CONCLUSIONS

In this work, we aimed at comparing two lipid nanocarriers produced by a similar process and composed with the same excipients in order to enhance the bioavailability of ferrocenyl tamoxifen derivative (Fc-diOH) in a 9L subcutaneous tumour model. Lipid nanocapsules exhibited great advantages compared to swollen micelles. Quantitatively, LNC were better internalised by glioma cancer cells compared to micelles; they were less toxic to healthy cells in culture and they could be loaded by hydrophobic molecules with high drug loading levels. Fc-diOH-loaded LNC showed interesting cytotoxic effects on 9L glioma cells with an IC_{50} equivalent to $0.6\mu\text{M}$, and furthermore, this organometallic compound was not active on normal brain cells in a concentration range $< 10\mu\text{M}$. Promising *in vivo* results were obtained after intratumoural s.c administration of this new drug-carrier as it dramatically reduced the tumour mass and glioma volume.

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